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(54) Title: METHOD FOR UTILIZING NEUTRAL LIPIDS TO MODIFY IN VIVO RELEASE FROM MULTIVESICULAR LIPOSOMES (57) Abstract <p>The rate of release of encapsulated active compound from a multivesicular liposomal (MVL) formulation is modified by selection of a neutral lipid component. A family of MVL formulations containing different slow:fast release neutral lipid molar ratios displays different release rates depending upon the molar ratio of the fast release neutral lipid to the slow release neutral lipid in each member. Incubation in plasma or a plasma-like medium at <i>in vivo</i> temperatures so as to obtain a release rate curve for each allows selection from among the members of the family of a liposomal formulation with a desired rate of release <i>in vivo</i>.</p>		

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METHOD FOR UTILIZING NEUTRAL LIPIDS TO MODIFY
IN VIVO RELEASE FROM MULTIVESICULAR LIPOSOMES

5 Background of the Invention

This invention relates to liposomal formulations of compounds such as drugs. More particularly this invention relates to methods of modifying the *in vivo* rate of release of encapsulated compounds from
10 multivesicular liposomes by the choice of the neutral lipid in the liposomal formulation.

When phospholipids and many other amphipathic lipids are dispersed gently in an aqueous medium they swell, hydrate, and spontaneously form multilamellar
15 concentric bilayer vesicles with layers of aqueous media separating the lipid bilayers. These systems are commonly referred to as multilamellar liposomes or multilamellar vesicles (MLV), and usually have diameters of from 0.2 to 5 μm . Sonication of MLV results in the
20 formation of small unilamellar vesicles (SUV) bounded by a single lipid bilayer with diameters usually in the range of from 20 to 100 nm, containing an aqueous solution. Multivesicular liposomes (MVL) differ from MLV- and SUV in the way they are manufactured, in the random,
25 non-concentric arrangement of aqueous-containing chambers within the liposome, and in the inclusion of neutral lipids necessary to form the MVL.

Various types of lipids differing in chain length, saturation, and head group have been used in liposomal
30 drug formulations for years, including the unilamellar, multilamellar, and multivesicular liposomes mentioned

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above. The neutral lipids used in the manufacture of multivesicular liposomes to date have been primarily limited to triolein and tricaprylin.

One of the major goals of the field is to develop liposomal formulations for controlled *in vivo* release of drugs and other active agents of interest. Certain drugs need to be released fairly rapidly upon emplacement of the liposomal depot, and others require a relatively slow rate of release over a sustained period of time. Heretofore, the rate of release of a biologically active compound from a liposomal formulation has been modified by selection of the amphipathic lipid, the accepted membrane forming lipid, or by manipulation of the phospholipid/cholesterol molar ratio. Alternatively, such compounds as an acid or an osmolality spacer have been included in the aqueous solution for encapsulation to aid in modifying the rate of release of the encapsulated biologically active compound.

The control of release rates from liposomal formulations is complicated by the fact that many biologically active agents, such as proteins, need to be stored at reduced temperatures, i.e., about 4°C, to retain full activity. Unfortunately, some liposomal formulations that display excellent release rates at *in vivo* temperatures disintegrate rather rapidly at such storage temperatures.

Thus, the need exists for more and better methods for selecting liposomal formulations that maximize control over the rate of release of the encapsulated active compound while simultaneously affording shelf life stability for long periods of time at storage temperatures of about 4°C, for example 2 to 10°C.

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Summary of the Invention

In general, the invention features a method for modifying the rate of release of a biologically active compound, such as a drug, that is encapsulated in a multivesicular liposomal formulation by utilizing in the formulation a neutral lipid component having a selected molar ratio of a slow release neutral lipid to a fast release neutral lipid, wherein the proportion of the fast release neutral lipid in the molar ratio is increased to increase the rate of release of the biologically active compound. Alternatively, the proportion of the slow release neutral lipid in the molar ratio can be increased to decrease the rate of release of the biologically active compound. Generally, the slow:fast neutral lipid molar ratio is in the range from about 1:1 to 0:1, for example 1:4 to 1:100, or 1:4 to 1:27, and the molar ratio of the neutral lipid component to the total lipid component (all the lipids in the liposome) is in the range from about 0.01 to about 0.21.

For modifying the *in vivo* release rate, the melting point of the neutral lipid component preferably is at or below the *in vivo* temperature at which the formulation is to be used, as well as at or below the temperature at which the formulation is to be stored.

Slow release neutral lipids useful in the new method of this invention are, for example, triolein, tripalmitolein, trimyristolein, trilaurin, and tricaprin with triolein being most preferred. Useful fast release neutral lipids include, e.g., tricaprylin and tricaproin, and mixtures thereof. However, tricaproin and other similar lipids are usually not used as the sole neutral lipid in a formulation of multivesicular liposomes intended for use *in vivo*.

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In another embodiment, the present invention provides a liposomal composition comprising a therapeutically effective amount of a biologically active compound encapsulated in a multivesicular liposome formulation wherein the formulation comprises a neutral lipid component comprising a molar ratio of slow release neutral lipid to fast release neutral lipid from about 1:1 to 1:100, for example from about 1:3 to 1:54, 1:4 to 1:27, or from about 1:4 to 1:18.

10 In yet another embodiment, the invention features a method for selecting a multivesicular liposomal formulation for encapsulating a selected biologically active compound so as to obtain a desired release rate profile of the active compound *in vitro* and/or a desired
15 therapeutic release rate *in vivo*. In this embodiment of the invention, a family of MVL formulations that encapsulate the selected biologically active compound is prepared wherein each member of the family utilizes a neutral lipid component having a different slow:fast
20 neutral lipid molar ratio, generally in the range from 1:0 to 0:1. For example, a family of formulations utilizing slow:fast neutral lipid molar ratios of 1:0, 1:1, 1:4, 1:18, 1:27, 1:100, 0:1 can be prepared. Each member of the family of formulations is incubated in the
25 medium in which the desired rate of release is to be obtained, i.e., either in a storage medium at storage temperature or in human plasma, a plasma-like medium, or in a physiological medium into which the physiologically active substance is to be released, such as cerebrospinal
30 fluid (CSF) at body temperature. By this means a release rate profile is obtained for each formulation. Then the formulation having the slow:fast neutral lipid ratio that yields the desired release rate profile under the desired

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conditions for the selected biologically active substance is selected.

Unless otherwise defined, all technical and scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which this invention belongs. Although methods and materials similar or equivalent to those described herein can be used in the practice or testing of the present invention, the preferred methods and materials are described below. All publications, patent applications, patents, and other references mentioned herein are incorporated by reference in their entirety. In case of conflict, the present specification, including definitions, will control. In addition, the materials, methods, and examples are illustrative only and not intended to be limiting.

The practice of this invention provides the advantage that a formulation of multivesicular liposomes can be selected to have relatively rapid release *in vivo* that does not compromise the desire of slow release at storage conditions. The method of the invention, therefore, provides a rationale for obtaining a desired release rate through selection of the neutral lipid component used in manufacture of the MVL without compromising the desire for the formulation to have a slow release at storage conditions. Further, the control over the rate of release under *in vivo* conditions operates more or less independently of the composition of the aqueous phase encapsulated or the combination of the other lipids in the formulations.

This finding is particular to multivesicular liposomes since other types of liposomes do not contain neutral lipids in the lipid component and/or do not

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incorporate the neutral lipids into closely packed, non-concentric vesicles.

Other features and advantages of the invention will be apparent from the following detailed description, 5 and from the claims.

Brief Description of the Drawings

Figure 1 is a graph comparing the release rates of recombinant, human granulocyte colony stimulating factor (rhu G-CSF) from multivesicular liposomes (MVL) 10 formulated with different molar ratios of triolein to tricaprylin (∇ , 100:0; Δ , 50:50; \circ , 25:75; \square , 10:90; \diamond , 0:100) as the neutral lipid when incubated at 37°C in 60% human plasma in saline solution.

Figure 2 is a graph showing the results of a 15 pharmacodynamic study comparing the duration of the rhu G-CSF dependent elevation in peripheral blood leucocyte number of golden Syrian hamsters following subcutaneous injection of 100 ug/kg of rhuG-CSF in saline solution (∇), in a triolein-only, 100:0, MVL formulation (\circ), in a 20 triolein-only MVL formulation solubilized pre-injection with Tween™ 20 (Δ), and in a tricaprylin-only, 0:100, MVL formulation (\square).

Figure 3 is a graph comparing the release rates of rhu GM-CSF from MVL formulated with different molar 25 ratios of triolein to tricaprylin (Δ , 100:0; \circ , 25:75; \square , 10:90) as the neutral lipid when incubated at 37°C in 60% human plasma in saline solution.

Figure 4 is a graph showing a pharmacokinetic study of levels of rhu GM-CSF in venous blood, plasma 30 samples of mice following a subcutaneous injection of 1 mg/kg rhu GM-CSF in the triolein-only, 100:0, MVL formulation (\circ) and in the 25:75, triolein:tricaprylin

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MVL formulation (\square). The rhu GM-CSF level in EDTA-plasma was determined by ELISA. LOQ is the limit of quantitation.

Figure 5 is a graph showing the release rates of
5 rhu IGF-1 from multivesicular liposomes formulated with various triglycerides as the neutral lipid component when incubated at 37°C in 60% human plasma in saline solution. The neutral lipids used in MVL manufacture were: (\square) triolein, (O) tripalmitolein, (Δ) tricaprylin, (∇)
10 trilaurin, and (\diamond) tricaprln.

Figure 6 is a graph showing the results of a pharmacokinetic study of levels of rhu IGF-1 in serum of rats following subcutaneous injection of 6.25 mg/kg rhu IGF-1 in the tripalmitolein MVL formulation (O) and in
15 the tricaprylin MVL formulation (Δ). The rhu IGF-1 level in serum was determined by ELISA.

Figure 7 is a graph showing the release of rhu insulin and coencapsulant ^{14}C -sucrose from MVL manufactured with the neutral lipid, triolein or
20 tricaprylin when incubated at 37°C in saline solutions containing 60% human plasma. (\square) sucrose retained by triolein MVL formulation; (O) insulin retained by triolein MVL formulation; (Δ) sucrose retained by tricaprylin MVL formulation; and (∇) insulin retained by
25 tricaprylin MVL formulation.

Figure 8 is a graph comparing the release rates of morphine from MVL formulated with different molar ratios of triolein to tricaprylin as the neutral lipid when incubated at 37°C in 60% human plasma in saline solution.
30 (\square) 10:0, triolein:tricaprylin, 10 batches; (\odot , O) 1:4, triolein:tricaprylin, 2 batches; (Δ) 1:9, triolein:tricaprylin; (∇) 0:10, triolein:tricaprylin.

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Figure 9 shows results of a pharmacokinetic study of morphine MVL formulations manufactured with different molar ratios of triolein to tricaprylin and injected into the epidural space of Beagle dogs. Morphine release by the MVL was determined by measuring the level of morphine in the adjacent, dura membrane-separated, cerebral spinal fluid. (◇) 5 mg morphine (sulfate) in saline solution; (▽) 40 mg of morphine in the 10:0, triolein:tricaprylin MVL formulation; (O) 20 mg of morphine in the 1:4, triolein:tricaprylin MVL formulation; (□) 20 mg of morphine in the 1:9, triolein:tricaprylin MVL formulation; and (Δ) 20 mg of morphine in the 0:10, triolein:tricaprylin MVL formulation.

Figure 10 is a graph summarizing in an Arrhenius transformation the results of a study determining the effect of storage temperature on release rate of morphine from 2 batches of the 1:9, triolein:tricaprylin MVL formulation. The MVL were stored in normal saline solution at 4°C, 26°C, 37°C, and 41°C. The ordinate is the rate of morphine release from MVL expressed in terms of amount released per day as a percentage of total amount of morphine in the MVL suspension; the abscissa is $1/\text{storage temperature} \times 10^4$ ($^{\circ}\text{K}$)⁻¹.

Figure 11 is a graph showing cytosine arabinoside (AraC) retained in MVL incubated in human plasma at 37°C. The MVL formulations used as the neutral lipid component (□) triolein only; (O) 1:4, triolein:tricaprylin; (▽) 1:9, triolein:tricaprylin; (x) 1:18 triolein:tricaprylin; (Δ) 1:27, triolein:tricaprylin; and (◇) tricaprylin only.

Figure 12 is a graph showing the effect the neutral lipid ratio on release of cytosine arabinoside from MVL incubated in human plasma at 37°C when the MVL

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were formulated with the major phospholipid component, DOPC, replaced with DSPC. The formulations were (□) DOPC and triolein only; (Δ) DOPC 1:9, triolein:tricaprylin; (◇) DOPC and tricaprylin only; (○) DSPC and triolein only; (∇) DSPC 1:9, triolein:tricaprylin; and (+) DSPC and tricaprylin only.

Figure 13 is a graph showing the effect of the neutral lipid ratio on release of ¹⁴C-sucrose from MVL incubated in human plasma at 37°C when the MVL were formulated with the major phospholipid component, DOPC, replaced with DEPC. The DOPC formulations were (□) triolein only; (Δ) 1:9, triolein:tricaprylin; and (○) tricaprylin only. The DSPC formulations were (∇) triolein only; (+) 1:9, triolein:tricaprylin; and (◇) tricaprylin only.

Figure 14 is a graph showing the effect of using tricaproin as the neutral lipid component alone or in combination with triolein on the release of ¹⁴C-sucrose from MVL incubated in human plasma at 37°C. The formulations were (○) triolein only; (Δ) 1:4 triolein:tricaproin; (∇) 1:9 triolein:tricaproin; (◇) 1:18 triolein:tricaproin; and (+) tricaproin only.

Figure 15 is a graph showing the in vitro release of a 15-mer oligonucleotide from MVL prepared with triolein (□) or tricaprylin (○) as the neutral lipid. The MVL were incubated in rat cerebral spinal fluid (CSF) at 37°C.

Figure 16 is a graph showing the release during incubation in human plasma of ¹⁴C-sucrose from MVL also containing E. coli plasmid PBR 322 and lysine-hydrochloride. Sucrose release was used as a surrogate

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indicator of plasmid release. The MVL were manufactured with either (O) triolein or (Δ) tricaprylin as the neutral lipid.

Figure 17 is a graph showing the release of ¹⁴C-sucrose during incubation in human plasma of MVL manufactured with tripalmitolein and tricaprylin as the neutral lipid component. The neutral lipid ratio used in the MVL formulations were (O) tripalmitolein only; (+) 1:1 tripalmitolein:tricaprylin; (\diamond) 1:2 tripalmitolein:tri-caprylin; (∇) 1:4 tripalmitolein:tricaprylin; (Δ) 1:9 tripalmitolein:tricaprylin; and (\square) tricaprylin only.

Figure 18 is a graph showing the amount of tetracaine remaining at the subcutaneous injection site of mice injected with tetracaine containing MVL manufactured with a neutral lipid component of either (*) triolein; (X) 10:90, triolein:tricaprylin; (+) 5:95, triolein:tricaprylin; (\diamond) 2:98, triolein:tricaprylin; (∇) 1:99, triolein:tricaprylin; or (O) tricaprylin.

Figures 19A-D are graphs showing the release of MVL-encapsulated, biologically active compounds during storage in normal saline at temperatures of 2 - 8 (nominal 4), 25, 32, and 37°C. The MVL were manufactured with either tricaprylin (Figures 19A and 19C); or tricaprin (Figures 19B and 19D); as the neutral lipid component and with either cytosine arabinoside (Figures 19A and 19B); or morphine, Figures 19C and 19D) as the biologically active compound.

Figure 20 is an Arrhenius plot of the graphs in Figures 19A and 19B showing the dependence of cytosine arabinoside release rate on the storage temperature of MVL manufactured with (\square) tricaprylin, melting point (mp) 8°C; or (O) tricaprin, mp 31.5°C, as the neutral lipid

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component. The abscissa is the inverse of storage temperature, °K.

Detailed Description

A method is provided for modifying the rate of
5 release of a biologically active compound, such as a drug, encapsulated in a multivesicular liposomal formulation by selection of the neutral lipid, or combination of neutral lipids, used to manufacture the multivesicular liposomes (MVL).

10 There are at least three types of liposomes. The term "multivesicular liposomes (MVL)" as used throughout the specification and claims means man-made, 1-200 μm particles partially comprised of lipid membranes enclosing multiple non-concentric aqueous chambers. In
15 contrast, "multilamellar liposomes or vesicles" (MLV) have multiple "onion-skin" concentric membranes, in between which are shell-like concentric aqueous compartments. Multilamellar liposomes characteristically have mean diameters in the micrometer range, usually from
20 0.5 to 25 μm . The term "unilamellar liposomes or vesicles (ULV)" as used herein refers to liposomal structures having a single aqueous chamber, usually with a mean diameter range from about 20 to 500 nm.

Multilamellar and unilamellar liposomes can be
25 made by several relatively simple methods. The prior art describes a number of techniques for producing ULV and MLV (for example U.S. Patent No. 4,522,803 to Lenk; 4,310,506 to Baldeschweiler; 4,235,871 to Papahadjopoulos; 4,224,179 to Schneider, 4,078,052 to
30 Papahadjopoulos; 4,394,372 to Taylor 4,308,166 to Marchetti; 4,485,054 to Mezei; and 4,508,703 to Redziniak).

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By contrast, production of multivesicular liposomes requires several process steps. Briefly, the preferred method for making MVL is as follows: The first step is making a "water-in-oil" emulsion by capturing in
5 a lipid component composed of at least one amphipathic lipid and at least one neutral lipid in one or more volatile organic solvents for the lipid component, an immiscible first aqueous component and a biologically active substance to be encapsulated, and optionally
10 adding, to either or both the lipid component and the first aqueous component, an acid or other excipient for modulating the release rate of the encapsulated biologically active substances from the MVL. The mixture is emulsified, and then mixed with a second immiscible
15 aqueous component to form a second emulsion. The turbulence required for formation of the second emulsion is provided either mechanically, by ultrasonic energy, nozzle atomization, and the like, or by combinations thereof, to form solvent spherules suspended in the
20 second aqueous component. The solvent spherules contain multiple aqueous droplets with the substance to be encapsulated dissolved in them (see Kim et al., *Biochem. Biophys. Acta*, 728:339-348, 1983). For a comprehensive review of various methods of ULV and MLV preparation,
25 refer to Szoka, et al. *Ann. Rev. Biophys. Bioeng.* 9:465- - 508, 1980.

The term "solvent spherule" as used throughout the specification and claims means a microscopic spheroid droplet of organic solvent, within which are multiple
30 smaller droplets of aqueous solution. The solvent spherules are suspended and totally immersed in a second aqueous solution.

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The term "neutral lipid" means an oil or fat that has no membrane-forming capability by itself and lacks a hydrophilic "head" group.

The term "amphipathic lipid" means a molecule that
5 has a hydrophilic "head" group and hydrophobic "tail" group and has membrane-forming capability.

The term "zwitterionic lipid" means an amphipathic lipid with a net charge of zero at pH 7.4.

The term "anionic lipid" means an amphipathic
10 lipid with a net negative charge at pH 7.4.

The term "cationic lipid" means an amphipathic lipid with a net positive charge at pH 7.4.

As used herein, the "shelf life" of a liposomal formulation is related to the rate of release of the
15 encapsulated substance from a liposomal formulation in a storage solution, for instance normal saline (0.9% sodium chloride), at a storage temperature, for instance at 4°C.

In general, for making multivesicular liposomes, it is required that at least one amphipathic lipid and
20 one neutral lipid be included in the lipid component. The amphipathic lipids can be zwitterionic, anionic, or cationic lipids. Examples of zwitterionic amphipathic lipids are phosphatidylcholines, phosphatidylethanolamines, sphingomyelins etc. Examples
25 of anionic amphipathic lipids are phosphatidylglycerols, phosphatidylserines, phosphatidylinositols, phosphatidic acids, etc. Examples of cationic amphipathic lipids are diacyl trimethylammoniumpropane and ethyl phosphatidylcholine. Examples of neutral lipids are
30 triolein and tripalmitolein, trimyristolein and tricaprylin. In the new method, the release rate of the biologically active compound is modified by utilizing in manufacture of the multivesicular liposomes a neutral

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lipid component that provides the desired rate of release in the type of fluid in which the MVL are to be used.

For *in vivo* use, therefore, the release rate of the MVL must be determined in plasma or a plasma-like medium

5 because the release rate of the biologically active compound from the MVL for certain neutral lipids can differ greatly depending on whether the release is into saline or plasma.

As used herein, the term "neutral lipid component" means the neutral lipid, or mixture of neutral lipids, used in manufacture of the multivesicular liposomes.

As used herein, the term "plasma-like medium," means a synthetic solution that includes in addition to normal saline, at least some of the protein or lipid constituents of blood plasma or components of other biological fluids, such as cerebro-spinal fluid (CSF), or interstitial fluids. For instance, normal saline containing citrated human plasma or bovine serum albumin (BSA) is an example of a "plasma-like medium" as the term
15
20 is used herein.

The term "*in vivo* conditions" means actual injection or emplacement of MVL into a living body, and includes so-called "*ex vivo*" incubation of MVL in plasma or a plasma-like medium at body temperature (i.e., 37°C for humans).

Although the neutral lipid component can comprise a single neutral lipid, generally the neutral lipid component comprises a mixture of a slow release neutral lipid and a fast release neutral lipid in a molar ratio
30 range from about 1:1 to 1:100, e.g., from about 1:4 to 1:18, wherein the rate of release of the biologically active compound decreases in proportion with the increase in the ratio of the slow release neutral lipid to the

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fast release neutral lipid. For convenience, the molar ratio of the slow release neutral lipid to the fast release neutral lipid is referred to herein as "the slow:fast neutral lipid molar ratio."

5 The "slow release neutral lipid" used in the practice of this invention can be selected from triglycerides having monounsaturated fatty acid ester moieties containing from about 14 to 18 carbons in the acyl chain and generally having a molecular weight from
10 about 725 to 885, and those with saturated fatty acid ester moieties containing from about 10 to 12 carbons in the acyl chain and generally having a molecular weight from about 725 to 885; and mixtures thereof. Cholesterol esters such as cholesterol oleate and esters of propylene
15 glycol. The preferred slow release neutral lipids for use in the method of this invention are triolein, tripalmitolein, trimyristolein, trilaurin, and tricaprln, with triolein or tripalmitolein being most preferred. When *in vivo* use is contemplated, trilaurin (mp 46.5°C)
20 and other neutral lipids with a melting point above 37°C are generally used in the practice of this invention only in mixture with one or more other neutral lipids wherein the mixture has a melting point temperature at or below, and preferably below 37°C. One skilled in the art will
25 know how to determine the melting point of a mixture of lipids, such as a mixture of triglycerides.

 The "fast release neutral lipid" used in the practice of this invention can be selected from triglycerides having monounsaturated fatty acid ester
30 moieties containing from about 6 to 8 carbons in the acyl chain and having a molecular weight from about 387 to 471, and mixtures thereof. However, it has surprisingly been discovered that the use of a neutral lipid component

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in MVL containing one or more neutral lipids with an acyl chain of six or less carbons (especially use of tricaproin as the sole neutral lipid) results in rapid release of the encapsulated compounds upon contact with the *in vivo* environment. Therefore neutral lipids with an acyl chain of six or less carbons should be used only in combination with one or more neutral lipids having a longer chain acyl moiety. The preferred fast release neutral lipids are tricaprylin, and mixtures of tricaprylin and tricaproin, or mixed chain C₆ to C₈ triglycerides. Propylene glycol diesters with eight or ten carbon acyl moieties, cholesterol oleate, and cholesterol octanoate can also be used as neutral lipids.

A factor of equal importance to the molar ratio of neutral lipids is selection of a neutral lipid component having a melting point below the temperature at which the MVL is to be stored and/or used. As many biologically active compounds highly desirable in therapeutic applications require low storage temperature to prevent rapid deterioration, the neutral lipid component should be selected to have a melting point below the desired storage temperature as well as below the temperature at which the formulation will be used *in vivo*.

The results of storage temperature tests were determined by inspecting the particles microscopically and measuring by chemical assay the amounts of encapsulated material released. As is seen in these studies (Figure 20), MVLs stored at a temperature below the melting point of the neutral lipid component undergo a structural reorganization of the membranes that is, in some cases, accompanied by rapid release ("dumping") of the encapsulated contents. This phenomenon is referred to herein as "the melting point effect." The time to

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onset of the melting point effect depends upon the neutral lipid composition and the ingredients of the encapsulated aqueous phase. Certain encapsulated compounds, such as IL-2, appear to interact with MVLs in such a way as to delay by hours or even days, the onset of "freezing" at temperatures below the melting point of the neutral lipid, perhaps by influencing formation in the MVL of an intermediate, "meta-stable" state. However, even formulations with such delayed onset eventually undergo the morphological transition characteristic of the melting point effect. Examples 15 and 16 below illustrate the melting point effect on the release rates of encapsulated biologically active compounds from MVL stored at a temperature below the melting point (Figures 19A-D and 20). To distinguish between the two states of morphological transition, the delayed onset effect is referred to herein as "the temperature effect."

In selecting the neutral lipid component in accordance with the practice of this invention, it is generally preferred that the neutral lipid component have a melting point at or above the temperature at which the MVL are to be stored and/or used (to prevent rapid loss of the encapsulated active compound either during storage or during *in vivo* use) due to the melting point effect. The melting point temperature of a neutral lipid component comprising a mixture of neutral lipids, and hence the temperature of the melting point effect on MVL containing the neutral lipid component, can readily be determined by preparing the mixture of interest and subjecting it to progressively lower temperatures until the mixture is observed to "freeze." One method of performing this procedure is disclosed in J.B. Rossell,

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Advances in Lipid Research 5: 353-408, 1967. One skilled in the art will be aware of other approaches that can be used to obtain this information. However, it should be remembered that the melting point effect upon the

5 liposomal formulation as a whole can be influenced by the other lipids in the MVL as well as by the ingredients in the first aqueous solution.

Table 1 below lists the number of carbons in the acyl chains, the molecular weight, and melting point

10 temperatures of representative neutral lipids that can be used in the practice of this invention.

Table 1

The Physical Properties of Neutral Lipids					
15	Neutral lipid	Fatty Acid Ester	Mol. Wt.	Viscosity cP	M.P. °C
	<u>TriGlycerides</u>				
	Triolein	C18:1 9C	885	74	5
	Tripalmitolein	C16:1 9C	801		≤5
20	Trimyristolein	C14:1 9C	725	≤5	
	Trilaurin	C12	639		45.5
	Tricaprin	C10	555		31.5
	Tricaprylin	C8	471	20-28	8.3
	Tricaproin	C6	387		≤0
25	Captex 355	C8,C10 mixed	Avg. 496		≤5
	<u>Propylene Glycol Diester</u>				
	Captex 200	C8,C10 mixed	Avg. 345	9-13	≤5
30	<u>Cholesterol Ester</u>				
	Cholesterol Oleate	C18:1 9C	651		44-47
	Cholesterol Octanoate	C8	512		110

In one method of the invention, the release rate

35 of the biologically active compound is modified by utilizing in manufacture of the multivesicular liposomes a neutral lipid component comprising triolein or tripalmitolein, or a mixture thereof, as the slow release neutral lipid, and selecting a molar ratio of the slow

40 release neutral lipid to a fast release neutral lipid in the range from about 1:0 to 0:1. The rate of release of

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the active compound increases with the increase in the proportion of the fast release neutral lipid in the molar ratio. Generally the molar ratio of the neutral lipid component to the sum of all the lipids in the MVL

5 formulation is in the range from about 0.01 to about 0.21. The preferred fast release neutral lipid for use in such formulations with triolein and/or tripalmitolein is tricaprylin.

In addition to the melting point effect, which is
10 contributed in part by the neutral lipid component, the characteristics of the aqueous phase encapsulated in the MVL, particularly the chemical interaction of the active compound with the lipids in the MVL, can also influence the rate of release of the biologically active compound.
15 To take this additional factor into account during formulation, in one embodiment this invention provides a method of tailoring the neutral lipid component to the aqueous phase of interest.

In the first step of the method, to determine how
20 the neutral lipid component functions with any specific aqueous phase (i.e., one containing a biologically active compound of interest), a family of MVL formulations is made containing the aqueous phase of interest, wherein each member of the family of formulations contains a
25 different slow:fast release neutral lipid molar ratio of - the selected slow and fast release neutral lipids such that the family as a whole represents a graded progression of such ratios, for example 1:1, 1:2, 1:4, 1:9, 1:18; 1:27, 1:100, etc.

30 The *in vivo* release rates corresponding to the various slow:fast neutral lipid molar ratios embodied in the individual members of the family of MVL formulations is determined by separately incubating each member of the

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family *in vitro* in plasma or a plasma-like medium at *in vivo* temperature, i.e. 37°C for humans, for a period of hours, or even days.

Any of the methods illustrated in the Examples, or
5 others known to one of skill in the arts, can be used to determine at progressive time points the cumulative amount of one or more substance(s) encapsulated with the aqueous phase that has been released during incubation. For ease in making this determination, a radioactive
10 substance, such as ¹⁴C sucrose, can be included in the aqueous phase at the time of encapsulation. However, it is preferred to select the biologically active compound of interest as the substance whose release rate is monitored and recorded. It is recommended that the
15 release rate information be obtained in this manner for each member of the family of formulations being tested.

From the release rate information determined by this procedure, a graph showing a release curve, or "release rate profile" can be plotted for each member of
20 the family of formulations to show its individual *in vivo* release characteristics, with the ordinate of the graph indicating the cumulative amount of the substance of interest that has either been released or retained, and the abscissa indicating progressive time points at which
25 the amount released or retained is measured. A corresponding family of rate release curves is thus generated, with each curve of the family illustrating the release characteristics of its corresponding slow:fast neutral lipid molar ratio when used with the aqueous
30 phase being tested.

The skilled practitioner can then select the formulation having the most desirable release characteristics for the particular therapeutic

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application of interest to obtain the desired control over release of the substance of interest (i.e., a biologically active compound) so as to deliver a therapeutically effective amount of the active compound to the individual to be administered the MVL formulation. A skilled practitioner can thus select a MVL formulation, in particular one having the most advantageous slow:fast neutral lipid molar ratio, for delivering a therapeutically effective dose over the optimum period of time so as to maximize the therapeutic effect of the drug or other biologically active compound administered during therapy.

For instance, if it is desired to produce a MVL formulation that releases a particular active compound *in vivo* in a relatively short period of time, i.e., over several hours after administration, the neutral lipid component that yields a release curve indicating such delivery characteristics when stored *in vitro* in plasma, or a plasma-like composition, at about 37°C will be selected. The proportion of the fast release neutral lipid in the ratio will be comparatively large in this circumstance. On the other hand, when it is desired to produce a MVL formulation that releases its active compound *in vivo* over a relatively long period of time, i.e., over tens of hours after administration, even up to 200 hours post administration, the neutral lipid component that yields a release curve indicating such delivery characteristics when incubated under *in vivo* conditions will be selected. In this case the proportion of the slow release neutral lipid in the molar ratio will be comparatively large, and in some instances the neutral lipid component will contain no fast release neutral lipid at all.

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The shelf-life stability of the formulations should also be determined by incubation of the formulations in the contemplated storage medium at whatever storage temperature is required to assure
5 integrity of the biologically active compound for a suitable period of time. For convenience, the self-life stability tests can also be conducted in plasma or a plasma-like medium, but one skilled in the art will be able to substitute a different suitable storage medium,
10 such as normal saline, for use with the biologically active compound of interest, if desired. Since many biologically active compounds require storage at temperatures in the range from about 2 to 8°C, it is recommended that the shelf-life stability tests be
15 conducted at a temperature in this range.

These procedures are illustrated in the Examples of this application. For instance, in formulations containing mixtures of triolein and tricaprylin, when the neutral lipid component was held constant and incremental
20 increases in the ratio of triolein to tricaprylin were made, MVL formulations characterized by increasingly slower release were obtained, as is illustrated in Example 14 (Figure 18). In Example 13, a graded family of formulations encapsulating sucrose and lysine-HCl and
25 containing mixtures of tripalmitolein and tricaprylin were prepared. A graded family of formulations was created with tripalmitolein:tricaprylin molar ratios of 0:1, 1:0, 1:9, 1:4, 1:2, and 1:1 by holding constant the amount of tripalmitolein and making incremental increases
30 in the amount of tricaprylin. In this Example, increasingly more rapid release was obtained for each incremental increase in the proportion of tricaprylin in the neutral lipid component.

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It should particularly be noted that, unlike most other types of liposomes, accurate *in vivo* release characteristics regarding MVL formulations cannot be predicted from *in vitro* release studies conducted in saline. For instance, MVL formulated with tricaproin, a triglyceride having only 6 carbons in its acyl moieties, as the only neutral lipid were not stable under *in vivo* conditions (in solutions containing plasma or serum albumin at 37°C, but were stable under storage conditions (in saline at 2-8°C for up to a week). However, formulations containing tricaproin:triolein molar ratios of 4:1, 9:1, and 18:1 were stable under *in vivo* conditions for at least 4 days, and yielded a graded set of release rate curves (Figure 14).

In another embodiment, the present invention provides liposomal compositions comprising a therapeutically effective amount of a biologically active compound encapsulated in a multivesicular liposome formulation wherein the formulation comprises a neutral lipid component with a molar ratio of slow release neutral lipid to fast release neutral lipid in the molar ratio range from about 0:1 to 1:0, for example 1:1 to 1:100 and generally from about 4:1 to 27:1. The molar ratio of the neutral lipid component to the sum of the lipids in the MVL formulation is generally in the range from about 0.01 to about 0.21.

The preferred amphipathic lipids for use in making the multivesicular liposomes are phospholipids with even numbers of carbons in the carbon chain because such phospholipids are natural lipids found in the body and do not produce toxic metabolites. A representative list of amphipathic lipids preferred for use in the practice of this invention follows. Also included are abbreviations

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that may be used to refer to particular phospholipids in this application.

DOPC or DC18:1PC = 1,2-dioleoyl-*sn*-glycero-3-phosphocholine

DLPC or DC12:0PC = 1,2-dilauroyl-*sn*-glycero-3-phosphocholine

5 DMPC or DC14:0PC = 1,2-dimyristoyl-*sn*-glycero-3-phosphocholine

DPPC or DC16:0PC = 1,2-dipalmitoyl-*sn*-glycero-3-phosphocholine

DSPC or DC18:0PC = 1,2-distearoyl-*sn*-glycero-3-phosphocholine

DAPC or DC20:0PC =

1,2-diarachidoyl-*sn*-glycero-3-phosphocholine

10 DBPC or DC22:0PC = 1,2-dibehenoyl-*sn*-glycero-3-phosphocholine

DC16:1PC = 1,2-dipalmitoleoyl-*sn*-glycero-3-phosphocholine

DC20:1PC = 1,2-dieicosenoyl-*sn*-glycero-3-phosphocholine

DEPC or DC22:1PC = 1,2-dierucoyl-*sn*-glycero-3-phosphocholine

DPPG = 1,2-dipalmitoyl-*sn*-glycero-3-phosphoglycerol

15 DOPG = 1,2-dioleoyl-*sn*-glycero-3-phosphoglycerol

The term "biologically active compound" as used herein means a chemical compound that is known in the art as having utility for modulating biological processes so as to achieve a desired effect in modulation or treatment of
20 an undesired existing condition in a living being, such as a medical, agricultural or cosmetic effect. Thus, biologically active compounds are generally selected from the broad categories of medicaments, pharmaceuticals, radioisotopes, agricultural products, and cosmetics.

25 Therapeutic biologically active compounds, or drugs for encapsulation in the methods and compositions of this invention include anti-neoplastic agents, anti-infective agents, hormones, anti-depressives, antiviral agents, anti-nociceptive agents, anxiolytics and
30 biologics.

Representative examples of anti-neoplastic agents useful in the compositions and methods of the present

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invention include methotrexate, taxol, tumor necrosis factor, chlorambucil, interleukins, etoposide, cytarabine, fluorouracil and vinblastine.

Representative examples of anti-infective agents
5 useful in the compositions and methods of the present invention include pentamidine, metronidazole, penicillin, cephalixin, tetracyclin and chloramphenicol.

Representative examples of anti-viral agents
useful in the composition and methods of the present
10 invention include dideoxycytidine, zidovudine, acyclovir, interferons, dideoxyinosine and ganciclovir.

Representative examples of anxiolytics and
sedatives useful in the compositions and methods of the
invention include benzodiazepines such as diazepam,
15 barbiturates such as phenobarbital and other compounds
such as buspirone and haloperidol.

Representative examples of hormones useful in the
compositions and methods of the present invention include
estradiol, prednisone, insulin, growth hormone,
20 erythropoietin, and prostaglandins.

Representative examples of anti-depressives useful
in the compositions and methods of the present invention
include fluoxetine, trazodone, imipramine, and doxepin.

Representative examples of anti-nociceptives
25 useful in the compositions and methods of the present
invention include hydromorphone, oxycodone, fentanyl,
morphine and meperidine.

The term "biologics" encompasses nucleic acids
(DNA and RNA), proteins and peptides, and includes
30 compounds such as cytokines, hormones (pituitary and
hypophyseal hormones), growth factors, vaccines etc. Of
particular interest are interleukin-2, insulin-like
growth factor-1, interferons, insulin, heparin,

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leuprolide, granulocyte colony stimulating factor (GCSF), granulocyte-macrophage colony stimulating factor (GM-CSF), tumor necrosis factor, inhibin, tumor growth factor alpha and beta, Mullerian inhibitory substance, 5 calcitonin, and hepatitis B vaccine.

The biologically active compound can be employed in the present invention in various forms, such as molecular complexes or biologically acceptable salts. Representative examples of such salts are succinate, 10 hydrochloride, hydrobromide, sulfate, phosphate, nitrate, borate, acetate, maleate, tartrate, salicylate, metal salts (e.g., alkali or alkaline earth), ammonium or amine salts (e.g., quaternary ammonium), and the like. Furthermore, derivatives of the active substances such as 15 esters, amides, and ethers which have desirable retention and release characteristics, but which are readily hydrolyzed *in vivo* by physiological pH or enzymes, can also be employed.

As used herein the term "therapeutically effective 20 amount" means the amount of a biologically active compound necessary to induce a desired pharmacological effect. The amount can vary greatly according to the effectiveness of a particular active substance, the age, weight, and response of the individual host as well as 25 the nature and severity of the host's symptoms. Accordingly, there is no upper or lower critical limitation upon the amount of the active substance. The therapeutically effective amount to be employed in the present invention can readily be determined by those 30 skilled in the art.

It is believed that the neutral lipid component in MVL, which is unique to MVL among liposomal formulations, interacts with the *in vivo* environment in such a way as

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to affect the rate at which compounds encapsulated within the MVL are released. In particular, MVL having a neutral lipid component comprised of triglycerides with less than 6 carbons in the acyl moiety interact with the *in vivo* environment so as to become completely destabilized virtually upon contact with blood plasma. For this reason, saline solutions do not accurately mimic the effect of the *in vivo* environment on the drug release characteristics of MVL, but it has been discovered that *in vitro* release studies conducted using blood plasma or a plasma-like medium can be used to accurately determine the *in vivo* release characteristics of an MVL formulation.

The following examples illustrate the manner in which the invention can be practiced. It is understood, however, that the examples are for the purpose of illustration, and the invention is not to be regarded as limited to any of the specific materials or conditions therein.

20

Example 1

G-CSF-containing MVL

1. Manufacture

For manufacture of multivesicular liposomes (MVL)-containing granulocyte colony stimulating factor (G-CSF), the lipid combination solution contained (per ml chloroform): 11 mg DOPC, 2.3 mg DPPG, 8.7 mg cholesterol and either 2.4 mg (2.7 μ mol) triolein or 1.3 mg (2.7 μ mol) tricaprylin. Lipid solutions which contained four different molar ratios of the neutral lipids triolein and tricaprylin were prepared by mixing appropriate volumes of the triolein and tricaprylin containing lipid

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solutions. The molar ratios of triolein to tricaprylin were 100:0, 50:50, 25:75, 10:90, and 0:100.

The first aqueous phase solution for MVL formulations contained 174 mM glycine, 100 mM HCl, 0.001% Tween80™, and 100 ug/ml G-CSF, 1 ml was added to a vial containing 1 ml of the lipid combination and emulsified by fixing the capped vial in a horizontal configuration to the head of a vortex mixer (Scientific Products) and shaking at maximum speed (2400 oscillations/min.) for 6
10 minutes.

The final emulsion (2 ml) was divided and transferred to two vials containing 2.5 ml 3.2% glucose and 40 mM lysine. The emulsion was dispersed into microscopic droplets by fixing the capped vial in a
15 horizontal configuration to the head of a vortex mixer and shaking for 3 seconds at 2400 oscillations/min. The contents of the vial were transferred to a flask containing 5 ml of 3.2% glucose, 40 mM lysine. The chloroform was removed from the microscopic droplets or
20 spherules by transferring the flask to a 37°C gyrorotary water bath and flushing the surface of the suspension with nitrogen gas at a flow rate of 10 - 15 cfh for 10 minutes. Multivesicular liposomes in suspension containing encapsulated G-CSF were obtained.

25 The particle suspensions were diluted 1:4 with normal saline, and the particles were harvested by centrifugation at 800 X g for 10 minutes. The supernatant solution was removed by aspiration, and the particles were washed twice by resuspension in fresh,
30 normal saline solution and centrifugation. The final washed product was resuspended at 25% packed-particle volume per total volume and stored at 2-8°C for subsequent studies.

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2. In vitro release rate

The *in vitro* release rate of the MVL prepared as described above was determined by incubation in saline solutions containing 70% citrated-human plasma and 0.1% sodium azide at 37°C. G-CSF was determined in the centrifuge-collected particle fraction by solubilization of samples in 50% IPA and quantitation by high pressure liquid chromatography and UV detection using known methods.

10 The dependence of the *in vitro* release rate of G-CSF on the composition of the neutral lipid component used in manufacture of the multivesicular liposomes is shown in Figure 1. As the triolein to tricaprylin molar ratio was increased, the rate of release of G-CSF from
15 the multivesicular liposomes decreased.

3. In vivo release rate

The triolein and tricaprylin MVL formulations of G-CSF were evaluated in a pharmacodynamic model in Syrian Golden Hamsters. Exogenous G-CSF stimulates neutrophil (granulocyte) production which can be evaluated by
20 assaying blood samples for an increase in peripheral blood neutrophil number and correspondingly an increase in peripheral blood leukocyte number.

Therefore, the formulations containing tricaprylin-
25 or triolein were evaluated for release in a pharmacodynamic hamster model that measured peak and duration of excess leukocyte (granulocyte) production caused by rhu G-CSF (Cohen et al. 1987, *Proc. Natl. Acad. Sci. USA*, 84:2484-2488). In these studies the
30 subcutaneous injection of a solution of G-CSF was used as a control for bioequivalence of the encapsulated protein. The rapid-release formulation containing tricaprylin was

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also used as a control for bioequivalence of the encapsulated protein. First, the peak and duration of granulocyte increase upon subcutaneous injection of hamsters with formulations containing all tricaprylin (slow:fast molar ratio of 0:100) was compared against that caused by a solution of unencapsulated G-CSF and the longer-release duration triolein formulation (slow:fast mole ratio of 100:0). For each formulation, 3 to 5 hamsters received 75-100 ug G-CSF per kg. The results (Figure 2), are as predicted by the *in vitro* release studies. The tricaprylin formulation provided a rapid release of G-CSF and stimulated granulocyte production similar to that of the unencapsulated G-CSF solution. The triolein formulation had a lower (and later) peak and longer duration.

As a further control, a group of hamsters were injected with the triolein formulation solubilized with detergent (Tween 20™) immediately prior to injection. The granulocyte number found at 24 hours for the solubilized formulation was similar to that observed resulting from injections of the G-CSF-solutions or the formulation containing only tricaprylin as the neutral lipid (Figure 2).

Example 2

1. Manufacture

Multivesicular liposomes containing granulocyte/macrophage-colony stimulating factor (GM-CSF) were manufactured as described in Example 1, but using neutral lipid molar ratios of triolein to tricaprylin of 100:0, 25:75 and 10:90.

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2. In vitro release in human plasma at 37°C

The suspensions were prepared and incubated in human plasma at 37°C as described in Example 1. GM-CSF remaining encapsulated was determined by solubilization of the particle fraction in 50% IPA and quantitation by high pressure liquid chromatography and UV detection using known methods.

The results of the *in vitro* release assay (Figure 3) demonstrate that the graded replacement of triolein with tricaprylin results in graded increases in release rate.

3. In vitro pharmacokinetics

BALBc mice (aged 7 to 8 weeks and weighing approximately 20 grams) were administered subcutaneous injections of liposomes containing GM-CSF manufactured with either 100% triolein or a 25:75 ratio of triolein to tricaprylin. Blood samples were collected before the injection and at 1, 2, 4, and 7 days post injection, and the plasma was assayed for GM-CSF concentration using an ELISA kit. The formulation manufactured with 25:75 triolein to tricaprylin provided a higher peak level and a shorter duration of detectable rhu GM-CSF compared to the formulation manufactured with 100% triolein as the neutral lipid (Figure 4). These results are as predicted by the *in vitro* assay in human plasma at 37°C, and show that the rate of release of encapsulated GM-CSF is increased by addition of tricaprylin to the neutral lipid component.

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Example 3

Depo/IGF-1

1. Manufacture

Multivesicular liposomes were manufactured with
5 rhu IGF (recombinant human insulin-like growth factor),
with ¹⁴C-sucrose as an osmotic spacer, and ammonium
citrate as a buffer. The lipid combination solution
contained (per liter) 10.4 g DOPC, 2.1 g DPPG, 7.7 g
cholesterol, and the triglyceride component was either
10 2.1 g triolein, 1.9 g tripalmitolein, 1.5 g trilaurin,
1.3 g tricaprln, or 1.1 g tricaprylin (molar ratio,
0.34:0.07:0.52:0.06).

The first aqueous phase solution contained (per
ml) 16 mg rhu IGF-1 (Chiron), 7% sucrose, and 20 mM
15 ammonium citrate, pH 5. A first emulsion was made by
high-speed mixing of 5 ml of the lipid combination
solution with 5 ml of the aqueous phase solution at 9000
rpm for 9 minutes at 25-27°C. The emulsion was sheared
into microdroplets (spherules) by addition of 30 ml 40 mM
20 lysine, 4% glucose solution to the mixing vessel and
mixing at 6000 rpm for 1 min. The chloroform was removed
from the microscopic droplets or spherules by
transferring the suspension to a flask containing 70 ml
of 40 mM lysine, 3.2% glucose solution, placing the flask
25 in 37°C gyrorotary water bath, and flushing the surface
of the suspension with nitrogen gas at a flow rate of 70
cfh for 20 minutes to obtain the MVL particles in
suspension.

The suspensions were diluted 1:4 with normal
30 saline, and the particles were harvested by
centrifugation at 800 X g for 10 minutes at room
temperature. The supernatant solution was removed by

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aspiration, and the particles were washed twice by resuspension in fresh, normal saline solution and centrifugation.

2. In vitro release rates

5 The final washed product was resuspended at 25% packed-particle volume per total volume and stored at a temperature of 2-8, 25, 32, or 37°C for either 24 or 48 hours. The pellet fraction from the 25,000 X G X 2 minute centrifugation was solubilized and assayed by HPLC
10 for IGF-1 retained. Also, each of the IGF-1-containing formulations stored at 2-8°C was evaluated within 24 hours in the *in vitro* release assay described in Example 1 and the results are summarized in Figure 5. The formulations manufactured with triolein (C18:1) or
15 tripalmitolein (C16:1) showed a similar release rate profile. Greater than 70% of the encapsulated IGF-1 released in 7 days. The formulation manufactured with tricaprylin (C8) demonstrated a rapid release rate profile with nearly complete release of IGF-1 in 2 days.
20 The formulations manufactured with tricaprin (C10) or trilaurin (C12) released IGF-1 markedly more slowly than the standard triolein formulation, less than 50% released in 7 days. These results suggest that the acyl chain length of the triglyceride is not directly correlated
25 with the rate of release of encapsulated IGF-1 *in vitro*, because the release of the tricaprylin (C8) formulations was more rapid than that of the tricaprin (C10) or trilaurin (C12) formulations.

 It should be noted that storage of the trilaurin
30 formulations in saline for only a few days at 2-8°C resulted in morphological reorganization of the particles and an accompanying complete release of encapsulated

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materials. This effect would not be expected from the stability exhibited in the *in vitro* release assay at higher temperatures. This catastrophic effect was related to storage of the formulation at temperatures significantly lower than the freezing point of the neutral lipid. This effect is demonstrated in Examples 16 and 17 below.

3. In vivo pharmacokinetics

Male, Sprague-Dawley rats (weighing 250 to 300g) were given subcutaneous injections of the multivesicular liposome formulation containing IGF-1 that were manufactured with either tricaprylin or tripalmitolein as the neutral lipid. The tricaprylin formulation demonstrated a higher peak level of plasma rhu IGF-1 and a short release duration compared to the formulation manufactured with tripalmitolein (Figure 6). This result confirms the prediction of rapid release of multivesicular liposomes manufactured with tricaprylin based upon results of the *in vitro* release assay.

20

Example 4

1. Manufacture

For manufacture of multivesicular liposomes containing rhu-insulin, the lipid combination solution contained (per ml chloroform): 11 mg DOPC, 2.3 mg DPPG, 8.7 mg cholesterol and either 2.4 mg (2.7 μ mol) triolein or 1.3 mg (2.7 μ mol) tricaprylin as indicated.

The first aqueous phase solution formulations contained 7.5% 14 C-sucrose, 20 mM citric acid, 50 mM HCl and 5 mg/ml rhu-Insulin (E. Coli, Sigma Chemical Co., St. Louis, MO). A first emulsion was made by high-speed

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mixing of 4 ml of the lipid combination solution with 4 ml of the aqueous phase solution at 9000 rpm for 8 minutes at 25-27°C. The emulsion was sheared into microdroplets (spherules) by addition of a solution to
5 the mixing vessel of 20 ml 20 mM lysine, 4% glucose, and mixing at 3000 rpm for 1 min. The chloroform was removed from the microscopic droplets or spherules by transferring the suspension to a flask containing 30 ml of a solution of 20 mM lysine, 4% glucose at 37°C in a
10 gyrorotary water bath and flushing the surface of the suspension with nitrogen gas at a flow rate of 70 cubic feet per hour for 20 minutes to obtain the MVL particles in suspension.

The suspensions were diluted 1:4 with normal
15 saline, and the particles were harvested by centrifugation at 800 X g for 10 minutes. The supernatant solution was removed by aspiration, and the particles were washed twice by resuspension in fresh, normal saline solution and centrifugation. The final
20 washed product was resuspended at 25% packed-particle volume per total volume and stored at 2-8°C for subsequent studies.

2. In vitro release rates

The "in vitro" release assay was performed by
25 diluting 1 volume of stored suspension with 3.2 volumes of citrated, human plasma, and placing 0.6 ml of this suspension into microfuge tubes which were stoppered and incubated under dynamic conditions at 37°C. After 1, 3, 6, and 7 days, the tubes were centrifuged at 14,000 X g X
30 2 minutes, and the supernatant solution was transferred to another tube for bioassay. The pellet fractions of centrifuged samples were incubated in 1% Nonidet® NP-40

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(CalBiochem, San Diego, CA), 50 mM trifluoroacetic acid for 10 minutes at 37°C. The ¹⁴C sucrose and insulin retained by the pellet fraction was determined, respectively, by scintillation counting and reverse phase HPLC using known methods. The results of these studies showed that the multivesicular liposomes manufactured with triolein as the neutral lipid released both sucrose and insulin in an equivalent and linear fashion, with nearly complete release in 7 days. By contrast, the formulation manufactured with tricaprylin retained only 20 to 25% of the encapsulated sucrose and insulin after only 1 day of incubation in plasma (Figure 7).

Example 5

1. Manufacture

For manufacture of multivesicular liposomes containing morphine, a GMP-validatable, scalable process was used. The neutral lipid component molar ratios of triolein to tricaprylin were 1:4 or 1:9. Control formulations contained triolein or tricaprylin as the sole neutral lipid. The lipid combination solution contained (per liter) 10.2 g DOPC, 2.0 g DPPG, 7.6 g cholesterol, 2.1 g to 1.1 g triglyceride depending on the molar ratio of triolein:tricaprylin, (molar ratio, 0.34:0.07:0.52:0.06).

The first aqueous phase solution contained (per liter) 21 g morphine sulfate pentahydrate, 0.01 N hydrochloric acid. A first emulsion was made by high-speed mixing of 0.62 l of lipid combination solution with 0.9 l of aqueous phase solution at 8000 rpm for 30 minutes at 25-27°C. The emulsion was sheared into microdroplets (spherules) by transferring to a second

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mixing vessel containing 15 liter 4 mM Lysine, 5.9% glucose solution; and mixing at 1250-1300 rpm for 1.5 min at 45°C. Chloroform was removed from spherules by sparging the suspension for 50 min at 45°C in stepped intervals: 17 min at 15 l/min, 5 min at 40 l/min, 28 min at 10 l/min. The MVL particles were thus obtained in suspension. The particles in the final suspension were concentrated and washed free of unencapsulated morphine by either cross-flow- or dia-filtration with 25 l of normal saline solution. The final washed product was stored at 2-8°C for subsequent studies.

2. In vitro release profiles

The *in vitro* release assays were performed by a 1:9 dilution of suspensions which contained 8 to 15 mg of encapsulated morphine sulfate per ml into human plasma. The suspensions were incubated at 37°C under dynamic conditions. After 1, 2, 4, and 7 days, samples were diluted 1:4 with normal saline; the particles were sedimented by centrifugation at 800 X g X 10 min and the particle fraction was assayed to determine the amount of morphine retained by solubilization of the pellet fraction with 50% IPA and assay by UV spectrophotometry using known methods.

Figure 8 shows the release rate profile of morphine release for these formulations into human plasma. As shown in earlier examples, as the ratio of the triolein to tricaprylin increases, the rate and extent of morphine release decreases.

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3. In vivo pharmacokinetics

The *in vivo* release of the multivesicular liposomes containing morphine manufactured with triolein and tricaprylin alone or in combination was evaluated in the Beagle dog using an epidural injection, pharmacokinetic model. In these studies the level of morphine released from the liposomal formulation injected at a epidural site was determined in the plasma and at an adjacent intrathecal site (CSF, cerebral spinal fluid) separated from the epidural site by the spinal meningeal membrane. Only the CSF results are shown (Figure 9).

A correlation is found between the *in vitro* release results summarized in Figure 8 and the release rate profiles observed in the dog model (Figure 9). The *in vivo* tricaprylin-containing formulation releases very rapidly, with nearly complete release in 24 hours. The Mean Residence Time (MRT) for the 100% tricaprylin formulation was similar to that for injection of unencapsulated morphine, i.e., 2.3 h vs. 1.6 h. The inclusion of a small amount of triolein during manufacturing, i.e., 1:9 or 1:4 triolein:tricaprylin molar ratio slows the release rate, extending the release duration over 4 to 5 days, with MRTs of 13.2 h and 15.3 h, respectively. The tricaprylin containing formulations all release more rapidly than the formulation using triolein as the only neutral lipid, which had a MRT of 69 h in this model.

4. Storage Stability

The step-wise alteration in the neutral lipid composition of the MVL to provide a family of formulations with step-wise increase in the release rate profiles of bioactive compound does not seem to

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compromise the storage stability of the formulations provided that the formulations are stored near or above the melting point of the neutral lipid combination. Batches of the 10:90 triolein:tricaprylin morphine MVL
5 formulation, described above and which release rapidly both *in vitro* and *in vivo*, were evaluated for dependence of the release rate on temperature of storage. The MVL suspensions in saline storage solution were incubated at the normal storage temperature, 2-8°C (4°C nominal) and at
10 elevated temperatures, 26, 37, and 41°C. The results of these studies are shown in Figure 10, an Arrhenius plot, which plots the logarithm of the release rate against 1/Temperature (°K). The slope of the plot appears to be continuous. The release rate profile at high temperature
15 supports the observation that the MVL stored in saline solution at 2-8°C have a very slow release (about 1% of the encapsulated morphine per 100 days) and therefore can be expected to have a shelf-life in excess of a year if a criteria of 5 or 10% release of encapsulated material is
20 the limit for shelf-life. Further, it is also evident that a physiological matrix such as plasma (Figure 9) or the *in vivo* environment of the epidural space (Figure 9) greatly accelerates the release when compared to the release in saline solution at 37°C, i.e., 50% of the
25 encapsulated morphine released per day, versus less than-1% of encapsulated morphine per day in the latter.

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Example 6

Cytosine Arabinoside

1. Manufacture

Multivesicular liposomes containing cytosine
5 arabinoside (AraC) were manufactured with various
substitutions for the phosphatidylcholine component of
the lipid organic phase solution. The substitutions were
performed to determine the effect on the release rate
profile of changing the acyl component in the major
10 phospholipid in a MVL formulation containing either
triolein or tricaprylin as the neutral lipid.

In this first example, DOPC is used to demonstrate
that the release rate in a physiological medium from MVL
formulations containing AraC/HCl in the aqueous phase can
15 be modified by adjusting the triolein to tricaprylin
ratio. The lipid combinations contained (per 1200 ml)
122.4 ml DOPC at 100 mg/ml, 2.4 g DPPG, 9.12 g
cholesterol, 2.5 g triolein or 1.3 g tricaprylin, or a
mixture thereof yielding a molar ratio of triolein to
20 tricaprylin of 1:4, 1:9, 1:18, or 1:27.

The first aqueous phase solution contained 20
mg/ml cytosine arabinoside, 0.1 N HCl. A first emulsion
was made by high speed mixing of 10 ml lipid combination
and 10 ml of first aqueous phase solution at 9000 rpm for
25 9 min. The emulsion was sheared into microdroplets by
transfer of first emulsion to second mixing vessel
containing 200 ml of 3.2% glucose, 40 mM lysine and
mixing at 2100 rpm for 2.5 minutes. The chloroform was
removed by transferring suspension to two, 1-liter flasks
30 and flushing at 70 cfh. The final suspension was diluted
1:2 with saline and particles collected by centrifugation

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at 800 X g X 10 min washed 3 times, resuspended to 33% lipocrit, and then adjusted to 10 mg/ml.

2. In vitro release into human plasma

The *in vitro* release rate profiles of the cytosine arabinoside (AraC) MVL formulations were obtained by dilution of the suspension 1:9 into human plasma and incubation of samples at 37°C under dynamic conditions. At time points of 1, 2, 4, and 7 days, 1.2 ml of saline was added to triplicate 0.3 ml samples, and the particle fraction was collected by centrifugation at 16,000 X g X 2 min. The supernatant fraction was removed by aspiration, and the particle fraction was resuspended in 1 ml of 50% isopropyl alcohol, vortexed, incubated at 37°C for 10 min, centrifuged and then 0.06 or 0.2 ml of the supernatant was added to 1.0 ml of 0.1 N HCl. Cytosine arabinoside was determined by U.V. samples at 280 nm.

The *in vitro* release profiles measuring AraC retained by the formulations of multivesicular liposomes are shown in Figure 11. Release from the formulation having only tricaprylin as the neutral lipid was rapid. As the ratio of tricaprylin to triolein used in the manufacture of the MVL formulation increases, the rate of release of cytosine arabinoside by the MVL incubated in plasma decreases. Thus, a family of release rate curves with predictably increasing release rates is created by incremental increases in the amount of triolein in the triolein to tricaprylin ratio.

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Example 7

Effect of Substitution of Higher Transition
Temperature PhosphatidylCholines or Longer Chain Length
for DOPC in Formulations Containing Tricaprylin

5 The ranking in a family of *in vitro* release rate
profiles (as obtained in Example 6) with the greater
molar ratio of tricaprylin to triolein resulting in
faster release both *in vivo* and in *in vitro* models
(plasma at 37°C), remains consistent when a
10 phosphatidylcholine of higher phase transition
temperature or of increased chain length is substituted
for DOPC in the formulations of Example 6. In this
example distearoylphosphatidylcholine (DSPC, mp 55°C) was
substituted for DOPC (mp 0°C).

15 1. Manufacture

The manufacturing parameters were adjusted to
accommodate the higher mp of DSPC by performing
emulsification at 50 °C. The manufacture of emulsions
used for the DOPC control formulations was performed at
20 ambient temperature. In addition, the HCl concentration
of the first aqueous phase solution was increased 36%
over that in Example 6.

The lipid combination solution contained (per
liter) 10.2 g DOPC or 10.3 g DSPC, 2.1 g DPPG, 7.7 g
25 cholesterol, and the triglyceride component was either
1.1 g tricaprylin or 2.1 g triolein (molar ratio of
0.34:0.07:0.52:0.06). Mixtures of triolein and
tricaprylin were blended to provide the ratios of 1:4,
1:9, 1:18, 1:2 triolein to tricaprylin for use in the
30 formulations.

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The first aqueous phase contained (per ml) 20 mg cytosine arabinoside and 136 mM Hcl. An emulsion was made by high-speed mixing of 10 ml of the lipid combination solution with 10 ml of the aqueous phase solution using a 2 cm diameter blade in a stainless steel vessel at 9000 rpm for 8 minutes at room temperature (for formulations with DOPC) or 55°C (for formulations with DSPC). The emulsion was sheared into microdroplets by transfer into a 400 ml glass Mason jar containing 200 ml of 5% glucose and 40 mM lysine and, using a 4 cm diameter blade, mixing at 4000 rpm for 1.5 minutes at the same temperature as used for the first emulsification. Chloroform was removed by placing the container in a 37°C gyratory water bath and flushing the surface of the suspension with nitrogen gas at a flow rate of 70 cfh for 20 minutes.'

The suspensions were diluted 1:4 with normal saline and the particles were collected by centrifugation at 800 x g for 10 minutes at room temperature. The supernatant was removed by aspiration, and then the particles were washed twice by resuspension in normal saline solution and centrifugation. The final washed pellet was resuspended in normal saline solution and adjusted to 10 mg/ml of cytosine arabinoside.

2. In vitro release profiles

The *in vitro* release assay of AraC from the MVLs was performed in human plasma as described in Example 6 above. As shown in Figure 12, in MVL in which the higher melting point DSPC was substituted for DOPC, a family of graded release rate profiles was obtained by varying the molar ratio of tricaprilyn to triolein, with the faster release formulations containing a higher molar ratio of

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tricaprylin to triolein. As has been shown previously for other formulations of MVL, an increase in hydrochloric acid concentration in the aqueous phase solution (as compared with that contained in the MVL of Example 6) can slow the release of the active substance *in vitro*.

Example 8

Sucrose

1. Manufacture

10 In this example, the effect of tricaprylin on the release rate was tested for formulations containing 4% sucrose as the active agent in formulations having dieucrylphosphatidylcholine (DEPC, mp (0°C), a 22 carbon chain length phosphatidylcholine, substituted for
15 dioleolyphosphatidylcholine (DOPC, mp (0°C), a 18 carbon chain length phosphatidylcholine.

The lipid solution contained (per liter) either 10.2 g DOPC or 11.0 g DEPC and 2.1 g DPPG, 7.7 g cholesterol, and the triglyceride component was either
20 1.1 g tricaprylin or 2.1 g triolein (molar ratio of 0.34:0.07:0.52:0.06). For mixtures of the neutral lipid, triolein- and tricaprylin-containing lipid combinations were blended to provide these triolein to tricaprylin molar ratios.

25 The first aqueous phase contained 4% Sucrose (Spectrum USP/NF, Los Angeles, CA) and was spiked with 40 uL of ¹⁴C sucrose. A first emulsion was made by high-speed mixing of 5 ml of the lipid combination solution with 5 ml of the aqueous phase solution using a 2 cm
30 diameter blade in a stainless steel vessel at 9000 rpm for 10 minutes at room temperature. The emulsion was

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sheared into microdroplets by transfer to a 400 ml glass Mason jar containing 200 ml of 4% glucose and 4 mM lysine for 2 minutes, using a 4 cm diameter blade and mixing at 3500 rpm. Chloroform was removed from the droplets by transferring the suspension to a 1 liter culture flask placed in 37°C gyratory water bath and flushing the surface of the suspension with nitrogen gas at a flow rate of 70 cfh for 20 minutes.

The particle suspensions were diluted 1:2 with normal saline, and the particles were collected by centrifugation at 800 x g for 10 minutes at room temperature. The supernatant was removed by aspiration, and the particles were washed twice by resuspension in normal saline solution and centrifugation. The final, washed particle pellet was resuspended in normal saline solution and adjusted to approximately 33% lipocrit.

2. In vitro plasma release studies

For *in vitro*, plasma release studies, the suspensions were diluted 1:10 in human plasma with 0.1% sodium azide. Triplicate aliquots of 300 uL were incubated in 1.5 ml screw-top Eppendorf tubes and harvested on days 0, 1, 2, 3, and 4. Samples were harvested by pulling tubes from the incubator at random, labeling the tube with day of pull, diluting the contents with 1.2 ml of normal saline solution, and centrifuging at 27,000 x g for 5 minutes in a microfuge. The supernatant was carefully aspirated away from the particle pellet. The pellet fraction was resuspended in 1 ml of 50% IPA by vortexing, incubating at 37°C for 10 minutes, and then vortexing. A 50 ul sample was then diluted with 3 ml of scintillation fluid in a

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scintillation vial, the vial was shaken vigorously and sucrose was determined by scintillation counting.

As can be seen from the data contained in Figure 13, the formulation containing only tricaprylin released all encapsulated sucrose within one day when incubated in plasma. The ratio of triolein: tricaprylin of 1:18 was required to achieve an intermediate rate of release for an MVL formulation with this aqueous phase when DEPC replaced DOPC.

10

Example 9

In this example, tricaproin (C6) was substituted for tricaprylin (C8) as a release rate modifying neutral lipid.

1. Manufacture

15 The lipid combination solution contained (per liter) a combination of 10.2 g, 2.1 g DPPG, 7.7 g cholesterol, and the triglyceride component was either 0.9 g tricaproin or 2.1 g triolein (molar ratio of 0.34:0.07:0.52:0.06). Mixtures of the lipid solutions
20 containing triolein and tricaproin, were blended to provide lipid solutions containing molar ratios of triolein to caproin of 1:4, 1:9 and 1:18. These formulations were manufactured and tested as described in Example 8.

25 The first aqueous phase contained 4% Sucrose (Spectrum USP/NF) and was spiked with 40 uL of ¹⁴C Sucrose (ICN lot#54661027). A first emulsion was made by high-speed mixing of 5 ml of the lipid combination solution with 5 ml of the aqueous phase solution using a 2 cm
30 diameter blade in a stainless steel vessel at 9000 rpm for 10 minutes at room temperature. The second

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emulsification was performed in a 400 ml glass Mason jar containing 200 ml of 4% glucose and 4 mM lysine, using a 4 cm diameter blade and mixing at 3500 rpm for 2 minutes. Chloroform was removed by transferring the contents of the jar to a 1 liter culture flask placed in 37°C gyrorotary water bath and flushing the surface of the suspension with nitrogen gas at a flow rate of 70 cfh for 20 minutes.

The suspensions were diluted 1:2 with normal saline, and the particles were harvested by centrifugation at 800 x g for 10 minutes at room temperature. The supernatant was removed by aspiration, and the particles were washed twice by resuspension in normal saline solution and centrifugation. The final washed pellet was resuspended in normal saline solution and adjusted to approximately 33% lipocrit wherein lipocrit in percent is the volume occupied by the liposomes divided by the total volume of the liposome suspension multiplied by one hundred. The yield for each variation in the neutral lipid was greater than 50%. Following manufacture the free sucrose concentration at 33% lipocrit was approximately 3% of the total sucrose concentration.

2. In vitro release profiles

For *in vitro* plasma release studies, the suspensions were diluted 1:10 in human plasma. Triplicate aliquots of 300 uL were incubated dynamically in 1.5 ml screw-top Eppendorf tubes and harvested on days 0,1,2,3, and 4. Samples were harvested by pulling tubes from the incubator at random, labeling the tube with the day of the pull, diluting the contents with 1.2 ml of normal saline solution, and centrifuging at 27,000 x g

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for 5 minutes in microfuge. The supernatant was carefully aspirated away from the pellet. The pellet fraction was resuspended in 1 ml of 50% IPA by vortexing, incubating at 37°C for 10 minutes, and then vortexing again. A 50 ul sample was then diluted with 3 ml of scintillation fluid in a scintillation vial, the vial was shaken vigorously, and ¹⁴C-sucrose radioactivity was determined by scintillation counting.

As shown in Figure 14, the substitution of tricaproin for tricaprylin in mixtures containing triolein as a release rate modifying neutral lipid combination results in formulations having a graded family of release rates for various triolein:tricaproin molar ratios. The greater the molar ratio of tricaproin to triolein, the more rapid the release of sucrose. There is a distinguishing difference between tricaproin and tricaprylin containing formations. With this aqueous phase, i.e., containing sucrose as the encapsulated active agent, the multivesicular particles manufactured using only tricaproin underwent a physical transformation and released their contents within 5 minutes of dilution into human plasma at room temperature. Dilution into saline solution containing 0.5% bovine serum albumin had the same effect. By contrast, the formulations containing only tricaprylin as the neutral lipid generally required 12 or more hours of incubation in plasma at 37°C for complete release of the active agent. Despite the instability of the tricaproin only formulations in human plasma or saline at room temperature. The formulations were stable during storage at 2-8°C in saline for at least a week.

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Example 10

Antisense Oligonucleotides

This example illustrates use of the method of the invention to encapsulate antisense oligonucleotides.

5 1. Manufacture

The first aqueous phase solution contained (per ml) 5, 10 or 20 mg of an IL-6 antisense oligonucleotide (donated by Leu Neckers, NIH, Bethesda, MD), which in some studies was biotinylated, and 5% mannitol.

10 Hydrochloric acid (0.1 ml of 1 N) was added to a vial containing 1 ml of the lipid combination of Example 1 and the combination was emulsified by fixing the capped vial in a horizontal configuration to the head of a vortex mixer (Scientific Products) and shaking at 2400
15 oscillations/min for 1 minute. The remainder of the first aqueous phase solution (0.9 ml 5% mannitol containing 10 mg antisense oligonucleotide) was added to the vial, and emulsification was continued for 5 minutes.

The final emulsion (2 ml) was divided and
20 transferred to two vials containing 2.5 ml 3.2% glucose, and 40 mM lysine. The emulsion was dispersed into microscopic droplets by fixing the capped vial in a horizontal configuration to the head of a vortex mixer - and shaking for 3 seconds at approximately 1200 rpm. The
25 contents of the vial were transferred to a flask containing 5 ml of 3.2% glucose, 40 mM lysine, and the chloroform was removed from the microscopic droplets or spherules by transferring the flask to a 37°C gyrorotary water bath, and flushing the surface of the suspension
30 with nitrogen gas at a flow rate of 15 cubic feet per hour for 10 minutes.

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The suspensions were diluted 1:4 with normal saline and the particles were harvested by centrifugation at 800 X g for 10 minutes. The supernatant solution was removed by aspiration, and the particles were washed
5 twice by resuspension in fresh, normal saline solution and centrifugation. The final washed product was resuspended at 25% packed-particle volume per total volume and stored at 2-8°C for subsequent studies.

The recovery of encapsulated oligonucleotide was
10 determined by diluting a sample of the suspension 1:1 with 0.1% SDS, incubating the sample in a boiling water bath for 2 minutes, and then diluting the sample (typically 1/20) into 0.1 N NaOH for determination of UV
absorption using a wavelength scan from 320 to 212
15 nmeters. The concentration of oligonucleotide in the sample was calculated by subtracting the measured A320 absorbance value from the A257 absorbance value. A sample of the first aqueous phase solution served as the standard, 17.6 (A257-1 cm) units per mg/ml.

20 2. In vitro release profiles

The *in vitro* release characteristics of multivesicular particles containing oligonucleotides were determined by measuring the amount of oligonucleotide remaining with particle fraction when incubated at 37°C -
25 in rat cerebral spinal fluid (CSF). Samples stored in normal saline were resuspended in the storage solution, and centrifuged at 750 X g for 10 minutes. The saline supernatant solution was removed by aspiration, and the particles were resuspended in rat CSF to concentrations
30 of 0.25 to 0.5 mg of the oligonucleotide per ml of CSF. The samples were incubated at 37 °C under static conditions. After 0, 1, 2, 3, and 7 days, samples of the

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particle/CSF suspensions were removed, diluted 10-fold in saline, centrifuged, and the supernatant was aspirated away from the particle fraction. The particle fraction was incubated in 0.1% SDS and diluted with 0.1 N NaOH,
5 and a UV absorbance spectrum of the oligonucleotide was obtained over 340 to 210 nmeter range. The amount of oligonucleotide retained by the particle fraction was determined as above.

As shown in Figure 15, the tricapyrylin formulation
10 did not release *in vitro* more rapidly, but rather had a greater overall release; the triolein-containing formulation stopped releasing the drug in rut CSF after about 2.5 days as compared with continued release by the tricapyrylin-containing formulation.

15 3. *In vivo* pharmacokinetics

When the antisense MVL formulations manufactured with tricapyrylin as the neutral lipid were tested *in vivo* by intrathecal injection in rats and samples of the CSF subsequently taken were examined microscopically, no
20 particles were evident in CSF after two days. The MVL particles manufactured with triolein were evident at two days but had a "shrunken" appearance. There was no evidence of free, native oligonucleotide by a 3'-end labeling assay.

25 To improve the sensitivity of the *in vivo* assay for oligonucleotide concentration in CSF, the oligonucleotide was biotinylated and the biotinylated oligonucleotide was formulated as described above in MVL using either triolein or tricapyrylin as the neutral
30 lipid. The recoveries of encapsulated biotinylated oligonucleotide were 78% for triolein and 82% for tricapyrylin-containing MVL. When studied *in vivo*,

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biotinylated oligonucleotide, found free in the CSF released from the tricaprylin-containing liposomes was below the limit of detection after 2 days. Free, biotinylated oligonucleotide was present in the rat sample CSF 4 days after administration of the triolein-containing formulations at a concentration of approximately 0.5 uM (results not shown). The *in vivo* data are consistent with the tricaprylin MVL rapidly releasing antisense oligonucleotide *in vivo*, and the triolein formulation providing a more sustained release of the oligonucleotides.

Example 11

Plasmid-containing MVL

1. Manufacture

For manufacture of multivesicular liposomes encapsulating the *E. coli* PBR322 plasmid, the lipid combination solution contained (per liter) 10.4 g DOPC, 2.1 g DPPG, 7.7 g cholesterol, 2.16 g triolein (mw 885.40) or 1.15 g tricaprylin (mw 470.7) (DOPC : DPPG : Cholesterol : triglyceride molar ratio, 0.34:0.07:0.52:0.06).

The first aqueous phase solution contained (per liter) 42 g ¹⁴C-sucrose (0.6 uCi per ml) 100 mmol lysine, 84 mmol hydrochloric acid, pH 7.4 and 20 ug/ml PBR322 plasmid (Promega, Madison WI). A first emulsion was made by high-speed mixing of 3 ml of lipid combination solution with 3 ml of aqueous phase solution at 9000 rpm for 9 minutes at 25-27°C. The emulsion was sheared into microdroplets (spherules) by addition of 20 ml of a 20 mM lysine, 4% glucose solution to the mixing vessel and further mixing at 4000 rpm for 2 min. The chloroform was

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removed from the microscopic droplets or spherules by transferring the suspension to a flask containing 30 ml of 20 mM lysine, 4% glucose solution at 37°C in a gyrorotary water bath, and flushing the surface of the
5 suspension with nitrogen gas at a flow rate of 70 liter per hr. for 20 minutes to form the MVL.

The MVL suspensions were diluted 1:4 with normal saline, and the particles were harvested by centrifugation at 800 X g for 10 minutes. The
10 supernatant solution was removed by aspiration and the particles were washed twice by resuspension in fresh, normal saline solution and centrifugation. The final washed product was resuspended to 25% packed-particle volume per total volume, and stored at 2-8°C for
15 subsequent studies.

2. In vitro release profile

The *in vitro* release assays were performed by a 1:2.5 dilution of suspensions which contained the multivesicular liposomes encapsulating PBR322 plasmid and
20 ¹⁴C-sucrose into human plasma. Previous studies had established that ¹⁴C-sucrose release was an adequate surrogate for estimating the release of the PBR322 plasmid from the MVL. The suspensions were incubated at 37°C under static conditions. At times of 0, 1, 2, 3, 6,-
25 10, and 17 days, samples were diluted 1:4 with normal saline, particles were sedimented by centrifugation at 800 X g X 10 min, and the particle fraction was assayed by dissolving samples in a scintillation counting solution and performing scintillation counting of the
30 amount of ¹⁴C-sucrose retained by the particle fraction.

The results of this study shown in Figure 16 indicate the PBR322 plasmid formulation using triolein as

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the neutral lipid was stable under simulated *in vivo* conditions and released about 30% of the encapsulated ¹⁴C-sucrose over a span of 17 days; whereas, the tricaprylin-formulated particles rapidly released their contents upon contact with human plasma at 37°C.

Example 12

In the following example sucrose and lysine-HCl used as excipients in the PBR322 plasmid formulation were encapsulated without additional active agent to yield an "excipient only" family of graded, sucrose release formulations using tripalmitolein:tricaprylin molar ratios as the neutral lipid.

1. Manufacture

For manufacture of multivesicular liposomes encapsulating only sucrose-lysine HCl, the lipid combination solution contained (per liter) 10.4 g DOPC, 2.1 g DPPG, 7.7 g cholesterol, 1.9 g to 1.0 g triglyceride depending on the molar ratio of tripalmitolein (mw 801, C16:1 9C):tricaprylin to yield a DOPC:DPPG:cholesterol:triglyceride molar ratio of 0.34:0.07:0.52:0.06. The molar ratios of tripalmitolein to tricaprylin prepared in the formulations of this example were 0:1, 1:0, 1:9, 1:4, 1:2, and 1:1.

The first aqueous phase solution contained (per liter) 42 g ¹⁴C-sucrose (1.0 µCi per ml), 100 mmol lysine, 90 mmol hydrochloric acid, pH 5.7. A first emulsion was made by high-speed mixing of 5 ml of lipid combination solution with 5 ml of aqueous phase solution at 9000 rpm for 9 minutes at 25-27°C. The emulsion was sheared into microdroplets (spherules) by addition of 20 ml of a 20 mM

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lysine, 4% glucose solution to the mixing vessel, and mixing at 5000 rpm for 1.5 min. The chloroform was removed from the microscopic droplets or spherules by transferring the suspension to a flask containing 30 ml of the 20 mM lysine, 4% glucose solution in a 37°C gyrorotary water bath, and flushing the surface of the suspension with nitrogen gas at a flow rate of 70 cubic feet per hr. for 20 minutes to obtain the multivesicular particles in suspension.

10 The suspensions were diluted 1:4 with normal saline, and the particles were harvested by centrifugation at 800 X g for 10 minutes. The supernatant solution was removed by aspiration and the particles were washed twice by resuspension in fresh, 15 normal saline solution and centrifugation. The final washed product was resuspended at 25% packed-particle volume per total volume and stored at 2-8°C for subsequent studies.

2. In vitro release profile

20 The "in vitro" release assays were performed by a 1:9 dilution into human plasma of suspensions which contained multivesicular liposome encapsulating ¹⁴C-sucrose. The suspensions were incubated at 37°C under dynamic gentle mixing. At time points of 0, 1, 3, 5, 8, - 25 and 12 days, samples were diluted 1:4 with normal saline, the particles were sedimented by centrifugation at 800 X g for 10 min, and the particle fraction was assayed by dissolving in scintillation counting solution and scintillation counting of the amount of ¹⁴C-sucrose 30 retained in the particles. The results of these studies (Figure 17) show that a 1:1 molar ratio of tripalmitolein to tricaprylin provided a somewhat slower release rate.

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than tripalmitolein alone. A graded family of release rates was obtained having faster release by increasing the proportion of tricaprylin in the neutral lipid component.

5

Example 13

Anesthetics

1. Tetracaine MVL formulations

For manufacture of MVL encapsulating tetracaine, the lipid combination solution contained (per ml
10 chloroform) 15.6 mg DOPC, 3.1 mg DPPG, 11.5 mg cholesterol, and 12.6 mg to 6.6 mg triglyceride depending on the molar ratio of triolein:tricaprylin. The lipophilicity of tetracaine was found to require that the concentration of lipid (68 $\mu\text{mol/ml}$) in the lipid
15 combination be increased 2 to 1.5 times higher to obtain satisfactory MVL formulations. The triglyceride was enriched as well; the molar ratio of DOPC:DPPG:cholesterol:triglyceride was 0.29 : 0.06 : 0.44 : 0.21. The molar ratios of triolein to tricaprylin
20 prepared in the formulations of this example were 1:0; 1:10; 0.5:10; 0.2:10; 0.1:10; 0.05:10; and 0:1. The first aqueous phase solution for encapsulation of tetracaine contained (per ml) 15 mg of tetracaine phosphate and 200-
mg of alpha-cyclodextrin polymer.

25 An aliquot of first aqueous phase solution (1 ml) was added to a vial containing 1 ml of the lipid combination and emulsified by fixing the capped vial in a horizontal configuration to the head of a vortex mixer (Scientific Products), and shaking at 2400
30 oscillations/min for 12 minutes.

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The final emulsion (1 ml) was divided and transferred to two vials containing 2.5 ml of a solution of 3.2% glucose, 5 mM lysine. The emulsion was dispersed into microscopic droplets by fixing the capped vial in a horizontal configuration to the head of a vortex mixer and shaking for 3 seconds at a setting of 600-800 oscillations/min. The contents of the vial were transferred to a flask containing 50 ml of a solution of 3.2% glucose, 5 mM lysine, and the chloroform was removed from the microscopic droplets or spherules by transferring the flask to a 37°C gyratory water bath, and flushing the surface of the suspension with nitrogen gas at a flow rate of one liter per min. for 20 minutes.

The suspensions were diluted 1:4 by volume with normal saline, and the particles were harvested by centrifugation at 800 X g for 10 minutes. The supernatant solution was removed by aspiration, and the particles were washed twice by resuspension in fresh, normal saline solution and centrifugation.

2. In vivo pharmacokinetics

The *in vivo* release characteristics of the multivesicular particles were determined in BalbC mice (aged 7 to 8 weeks; weighing approximately 20 grams) by subcutaneous injection in the abdomen region (100 ul). At time points of 0, 5, and 24 hours after injection, mice were sacrificed, the subcutaneous tissue was harvested, homogenized, and extracted, and extracts were assayed by HPLC using UV detection for the amount of tetracaine retained.

The desired *in vivo* release duration for the tetracaine MVL was 24 hours. Formulations which contained triolein only as the neutral lipid were found

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to be stable *in vivo* and released over too long a duration.

By including tricaprylin in the neutral lipid component, formulations with shorter duration and more
5 desirable pharmacokinetic profiles were obtained (Figure 18). The desired 24 hour release duration for the anesthetic was provided by a formulation with a 1 triolein: 100 tricaprylin ratio.

**The Relationship Between Neutral Lipid
10 Selection and Intended Storage Temperature.**

As shown in the following examples, the melting point of the neutral lipid is an important consideration in selection of the rate-modifying neutral lipid. However, other factors must also be taken into account,
15 for example, the composition of the first aqueous phase solution. The conclusion to these examples is that the freezing (melting or cloud) point of the neutral lipid or neutral lipid mixture should be above or near the storage temperature in order to assure storage stability. If
20 formulations are stored at temperatures significantly lower than the freezing point of the neutral lipid or mixture thereof, the MVL particles undergo a physical, morphological transition, which results in loss of internal structure and release of encapsulated materials.
25 This transition may occur within a few hours or over several days or weeks, depending on the composition of the first aqueous phase composition.

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Example 14

In the following example, MVLs were manufactured with either tricaprylin or tricaprin as the neutral lipid component. The freezing point of tricaprylin is 8°C and
5 that of tricaprin is 31 °C. The first aqueous phase contained either cytosine arabinoside or morphine sulfate in 0.1 N HCl. Aliquots of the final product were stored in saline at 2- 8, 25, 32, and 37 °C. The release of encapsulated materials was determined over the time of
10 storage.

1. Manufacture

For manufacture of MVLs, the lipid combination solution contained (per liter) 10.4 g DOPC, 2.1 g DPPG, 7.7 g cholesterol, and the triglyceride component was
15 either 0.93 g tricaprylin (C8) or 1.1 g tricaprin (C10) (molar ratio, 0.34:0.07:0.52:0.06). The first aqueous phase solution contained either (per ml) 20 mg cytosine arabinoside in 0.1 N HCl or 20 mg morphine sulfate pentahydrate in 0.1 N HCl.

20 For formulations encapsulating cytosine arabinoside, the first emulsion was made by high-speed mixing of 10 ml of lipid combination solution with 10 ml of aqueous phase solution at 9000 rpm for 14 minutes at - 25-27°C with a high shear blade. For formulations
25 encapsulating morphine, the first emulsion was made by high-speed mixing of 12.5 ml of the lipid combination solution with 7.5 ml of the aqueous phase solution at 9000 rpm for 14 minutes at 25-27°C. The first emulsions were sheared into microdroplets (spherules) by transfer
30 to a mixing chamber containing 200 ml of 40 mM lysine, 3.2% glucose solution, and mixing at 2100 rpm for 2.5

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min. The chloroform was removed from the microscopic droplets or spherules by transferring the suspension to a flask, placing the flask in 37°C gyratory water bath, and flushing the surface of the suspension with nitrogen
5 gas at a flow rate of 70 cfh for 20 minutes.

The suspensions were diluted 1:4 by volume with normal saline, and the particles were harvested by centrifugation at 800 X g for 10 minutes at room temperature. The supernatant solution was removed by
10 aspiration, and the particles were washed twice by resuspension in fresh, normal saline solution and centrifugation. The final washed product was resuspended at 33% packed-particle volume and stored.

The characterization of yields of encapsulated and
15 free (supernatant) cytosine arabinoside and morphine from the tricapylin and tricaprln MVL formulations was performed a few hours post-manufacture (Table 2). The yield of encapsulated cytosine arabinoside and morphine was acceptable, and the free (supernatant) concentrations
20 of cytosine arabinoside and morphine were low for both the tricapylin and tricaprln formulations.

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TABLE 2

	First Aqueous Phase Active Agent	Neutral Lipid	Yield, % of Initial Active	Storage Concen- tration, mg/ml	Supernatant Concen- tration, mg/ml
5	Cytosine Arabinoside	Tricaprylin	42	7.0	0.3
		Tricaprin	37	6.2	0.2
	Morphine Sulfate	Tricaprylin	46	11.2	0.3
		Tricaprin	36	8.9	0.2

2. Storage release profiles

The suspensions were stored at 2-8, 25, 32 or
 10 37°C. At time points of 24, 48 and 200 hours the
 suspensions were centrifuged at 25,000 X G for 2 minutes,
 and supernatant solutions were analyzed for content of
 cytosine arabinoside or morphine by 1:1 volume dilution
 with 50% isopropyl alcohol, vortexing, incubation at 37°C
 15 for 10 min, and centrifugation. The supernatant samples
 were analyzed by dilution into 0.1 N HCl and the
 concentration of cytosine arabinoside was measured by
 absorbance determined at 280 nm, or dilution into 0.1 N
 NaOH, and the morphine concentration was measured by
 20 absorbance determined at 298 nm.

The results of these storage-temperature-effect
 studies are shown in Figures 19A-D. Release rates from
 the MVL containing tricaprylin (melting point 8°C) are
 very slow at 2-8°C. Release rate increased with
 25 increasing storage temperature as would be expected as
 consistent with acceleration of release with elevation of
 temperature (Figures 19A and 19C). The AraC-MVL
 containing tricaprln (melting point 31°C), however,

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released the active agent at a very fast rate when stored below the melting point of the triglyceride. With storage of the tricaprln MVL at higher temperatures 25° and 32°, the release rate decreased, but with storage at 5 37° again increased (Figure 19B). In fact, the tricaprln-containing AraC-MVL particles stored below the melting point temperature of the neutral lipid tricaprln (31°C), were completely destabilized and released the encapsulated morphine over a few hours (Figure 19B).

10 The results for the storage study of cytosine arabinoside-containing MVL are shown in Figure 20 by an Arrhenius plot. The tricaprlylin MVL formulation showed an expected continuous linear relationship when log of the release rate is plotted versus temperature, 15 suggesting that a single process is responsible for release. On the other hand, the plot of the data for the tricaprlylin formulation was discontinuous, indicating that two processes are responsible for release in the temperature range studied. At higher temperatures above 20 the freezing point of tricaprln, the slope was as expected, i.e., rates increased with increased temperature of storage. The second process, the melting point effect, is observed below the freezing point of tricaprln wherein, the apparent rate increased with 25 decreasing temperature.

Again, comparison of the release rate profiles (19A-D) of particles having cytosine arabinoside encapsulated as a first aqueous phase component with particles having morphine sulfate encapsulated indicates 30 that onset of the destabililzing effect caused by storage of formulations below the melting point of the neutral lipid, called herein "the melting point effect," is dependent on the composition of the first aqueous phase

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solution. Onset of the melting point effect of tricaprln MVL during storage was observed to be rapid with cytosine arabinoside-containing formulations, (Figure 19B) but required several days for the morphine sulfate-containing formulations (Figure 19D). Further, the results of these studies suggest that the further below the freezing point the formulation is stored, the more rapid the onset of the melting point effect.

Example 15

10 In this example, the aqueous phase contained sucrose, cytosine arabinoside and 0.1 N HCl as an osmotic spacer. MVL were manufactured with triolein (mp 8°C), tricaprln (mp 31°C), or trilaurin (mp 46 °C) as the neutral lipid. The final product was stored at a
15 temperature of 2-8°C, 22, or 37°C, and the release of encapsulated materials was recorded during the time of storage.

1. Manufacture

For manufacture of MVL encapsulating cytosine
20 arabinoside with sucrose as an osmotic spacer in the presence of 0.1 N HCl, the lipid combination solution contained (per liter) 10.4 g DOPC, 2.1 g DPPG, 7.7 g - cholesterol, and the triglyceride component was either 1.1 g tricaprln (C10), 1.3 g trilaurin (C12), or 1.7 g
25 triolein (molar ratio of DOPC:DPPG:cholesterol:triglyceride was 0.34:0.07:0.52:0.06).

The first aqueous phase solution contained (per ml) 20 mg cytosine arabinoside and 51.3 mg sucrose in 0.1
30 N Hcl. A first emulsion was made by high-speed mixing of

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3 ml of lipid combination solution with 3 ml of aqueous phase solution at 9000 rpm for 8 minutes at 25-27°C. The emulsion was sheared into microdroplets (spherules) by addition of 20 ml of a 20 mM lysine, 4% glucose solution to the mixing vessel and mixing at 5000 rpm for 1.5 min. The chloroform was removed from the microscopic droplets or spherules by transferring the suspension to a flask containing 70 ml of a 40 mM lysine, 3.2% glucose solution, placing the flask in 37 C gyrorotary water bath and flushing the surface of the suspension with nitrogen gas at a flow rate of 70 cfh for 20 minutes to form the MVL particles in suspension.

The suspensions were diluted 1:4 by volume with normal saline, and the particles were harvested by centrifugation at 800 X g for 10 minutes at room temperature. The supernatant solution was removed by aspiration, and the particles were washed twice by resuspension in fresh, normal saline solution and centrifugation. The final washed product was resuspended at 25% packed-particle volume per total volume and stored at 2-8, 22, and 37°C for 1 or 6 days (data not shown). The suspension and the supernatant fraction obtained by centrifugation at 25,000 X G 2 minutes were analyzed for content of cytosine arabinoside by 1:1 volume dilution with 50% isopropyl alcohol, vortexing, incubation at 37°C for 10 min, and centrifugation. Then 0.06 or 0.2 ml of the sample was added to 1.0 ml of 0.1 N HCl, and cytosine arabinoside concentration was measured by absorbance determined at 280 nm.

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TABLE 3

Triglyceride Component	Storage Temp °C	Total AraC Encapsulated mg/ml	Supernatant AraC @24h mg/ml	Ratio of Supernatant to total (Sup/Total)
5 Triolein, mp 5°C	2-8	6.0	0.4	0.06
	22	5.6	0.3	0.05
	37	5.2	0.9	0.17
Trilaurin, mp 46°C	2-8	3.0	2.5	0.82
	22	3.1	2.0	0.65
	37	3.0	2.3	0.78
Tricaprin, mp 31°C	2-8	5.6	5.0	0.90
	22	5.4	4.8	0.90
	37	6.7	0.6	0.09

10 As shown by the data in Table 3, the product yield of the MVL formulated using each of the neutral lipids was at least 3.0 mg/ml, an acceptable yield. Inspection of the particles with white light microscopy showed that the particles were spherical and multivesiculated in
15 appearance immediately post-manufacture. However, within 24 hours of storage at temperatures below the melting point of the triglyceride, the particles changed in appearance. Associated with the change in appearance was significant loss of the encapsulated AraC to the storage
20 solution (supernatant) as can be seen by the data in column 3 of Table 3. Noteworthy, the formulation manufactured with tricaprin (mp. 31°C) did not change in appearance, or lose significant AraC when stored at 37°C; whereas the formulation with trilaurin (mp 46°C) did

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undergo a significant morphological change and loss of encapsulated active agent. Thus in formulating MVL for *in vivo* controlled and sustained delivery of the encapsulated active agent, the neutral lipid selected
5 should usually have a melting point below or near the intended storage temperature. A preferred formulation would maintain a supernatant/total ratio of less than 0.10 during storage.

Example 16

10 This example illustrates that certain aqueous phase solutions are interactive with the lipid layer membrane of MVLs and prevent freezing of the liposomes at storage temperatures below the melting point of the neutral lipid. In such cases, the morphological
15 transition of the particles and loss of encapsulated materials associated with storage below the melting point of the neutral lipid may occur very slowly, or disappear. Instead the release of encapsulated materials is associated with activation by storage temperature
20 increase.

1. Manufacture

For manufacture of MVL encapsulating rhu IGF with ¹⁴C-sucrose as the osmotic spacer and ammonium citrate as the buffer, the lipid combination solution contained (per
25 liter) 10.4 g DOPC, 2.1 g DPPG, 7.7 g cholesterol, and the triglyceride component was 1.3 g tricaprin (mp 31°C, C10) (with the molar ratio of DOPC:DPPG:cholesterol:triglyceride was 0.34:0.07:0.52:0.06).

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The first aqueous phase solution contained (per ml) 16 mg rhu IGF-1 (Chiron, Foster City, CA), 7% ¹⁴C-sucrose, and 20 mM ammonium citrate, pH 5. A first emulsion was made by high-speed mixing of 5 ml of lipid combination solution with 5 ml of aqueous phase solution at 9000 rpm for 9 minutes at 25-27°C. The emulsion was sheared into microdroplets (spherules) by addition of 30 ml of a 40 mM lysine, 4% glucose solution to the mixing vessel and mixing at 6000 rpm for 1 min. The chloroform was removed from the microscopic droplets or spherules by transferring the suspension to a flask containing 70 ml of a 40 mM lysine, 3.2% glucose solution, placing the flask in a gyrorotary water bath at 37°C, and flushing the surface of the suspension with nitrogen gas at a flow rate of 70 cfh for 20 minutes to obtain the MVL particles.'

The suspensions were diluted 1:4 with normal saline and the particles were harvested by centrifugation at 800 X g for 10 minutes at room temperature. The supernatant solution was removed by aspiration, and the particles were washed twice by resuspension in fresh, normal saline solution and centrifugation.

2. In vitro release rates

The final washed product was resuspended at 25% - packed-particle volume per total volume and stored at temperatures of 2-8, 25, 32, and 37°C for 24 or 48 hours. The pellet and supernatant fraction from the centrifugation at 25,000 X G for 2 minutes was assayed for content of IGF-1 (pellet fraction only) and ¹⁴C-sucrose.

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TABLE 4

Temperature, °C	Retained @ 24 hours		Retained @ 48 hours	
	¹⁴ C-Sucrose	IGF-1	¹⁴ C-Sucrose	IGF-1
2-8	1.00	1.00	0.98	0.98
5 25	0.95	0.97	0.91	0.94
32	0.90	0.96	0.74	0.86
37	0.83	0.91	0.56	0.75

The results of these studies summarized in Table 4 show that the contents of the first aqueous phase solution can prevent or slow the freezing effect which was shown in Example 16 to be associated with storage of MVLs containing trilaurin as the neutral lipid at a temperature below its melting point of 46°C. The lipids used and method of manufacture were identical in both formulations; however, the encapsulated aqueous phase components were different. This suggests that the composition of the first aqueous phase may modulate either the freezing point of the triglyceride or the melting point effect, for instance by preventing the neutral lipid from transitioning to an unstable structure or markedly slowing the freezing.

The release in plasma of the tricaprln- and trilaurin-containing MVL formulations (shown in Example 16) was markedly slower than from MVL manufactured with tricaprlylin, as shown in Table 4 and in later examples. It should be noted that all the plasma release assays conducted at 37°C were initiated within 24 hours of manufacture. The storage at 2-8°C for longer than a few days of the trilaurin, but not the tricaprln-containing formulations, resulted in morphological change in the

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appearance of the particles and release of encapsulated materials consistent with the "melting point effect".

Example 17

Other neutral lipids

5 A study series was performed wherein the neutral lipids were decane, dodecane, squalene, and alpha-tocopherol to determine the scope of neutral lipids that can be used to obtain multivesicular liposomal formulations.

10 1. Manufacture

 Multivesicular liposomes encapsulating a combination of glycine, sucrose, and Tris-EDTA were made wherein the lipid combination solution contained (per liter) 10.4 g DOPC, 2.1 g DPPG, 7.7 g cholesterol, and
15 the triolein component (6 mol % of lipid) was replaced with either decane, dodecane, squalene, or alpha-tocopherol, (molar ratio of DOPC:DPPG:cholesterol:neutral lipid was 0.34:0.07:0.52:0.06).

 The first aqueous phase solution contained 200 mM
20 glycine, 50 mM Sucrose, 1.8 mM Tris base, and 0.5 mM EDTA, pH 7.44, with an osmolarity of 268 mOsmol. A first emulsion was made by high-speed mixing of 3 ml of lipid combination solution with 3 ml of aqueous phase solution at 9000 rpm for 9 minutes at 25-27°C. The emulsion was
25 sheared into microdroplets (spherules) by the addition of 20 ml of a 20 mM lysine, 4% glucose solution to the mixing vessel and mixing at 4000 rpm for 1.0 min.

 Examination of the spherule suspensions under the microscope indicated that the spherules prepared with
30 each of these neutral lipids were normal in internal

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appearance as compared to controls prepared with triolein, tripalmitolein, or trimyristolein as the neutral lipid component.

The chloroform was removed from the microscopic droplets or spherules by transferring the suspension to a flask containing 30 ml of a 40 mM lysine, 3.2% glucose solution, placing the flask in 37°C gyrorotary water bath, and flushing the surface of the suspension with nitrogen gas at a flow rate of 70 cfh for 20 minutes to obtain the MVL particles.

Only MVL prepared with squalene as the neutral lipid survived the solvent removal step or subsequent washing of the particles and gave rise to normal-looking MVL particles after the wash step. During the solvent removal step, decane, dodecane and alpha-tocopherol spherules began to shrink, with lobes of light-refractile material emanating from their surface. Abruptly, the particles collapsed into a crenellated structure. In some cases a pellet, albeit small as compared to controls, was recovered from the wash step, and the particles did not have the appearance of multivesicular liposome compositions.

Other Embodiments

The foregoing description of the invention is exemplary for purposes of illustration and explanation. It should be understood that various modifications can be made without departing from the spirit and scope of the invention. Accordingly, the following claims are intended to be interpreted to embrace all such modifications.

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CLAIMS:

1. A method for modifying the rate of release of a biologically active compound encapsulated in a multivesicular liposome having a neutral lipid component
5 comprising:

(1) forming an emulsion from a) a lipid component comprising an organic solvent, an amphipathic lipid, and a neutral lipid component comprising a molar ratio of from 1:0 to 0:1 of a slow release rate neutral lipid to a
10 fast release rate neutral lipid, and b) an immiscible first aqueous component wherein at least one biologically active compound is incorporated into either the lipid component or the first aqueous component, or both;

(2) mixing the emulsion with a second aqueous
15 component to form solvent spherules, and

(3) removing the organic solvent from the solvent spherules to form multivesicular liposomes encapsulating the biologically active compound;

wherein the molar ratio of the slow release
20 neutral lipid to the fast release neutral lipid is decreased to increase the rate of release of the biologically active compound.

2. The method of claim 1, wherein the molar
25 ratio of the neutral lipid component to all the lipids in the liposome is in the range from about 0.01 to about 0.21.

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3. The method of claim 1, wherein the slow release neutral lipid is selected from the group consisting of triglycerides having a monounsaturated fatty acid ester containing from about 14 to 18 carbons
5 in the acyl chain, those having a saturated fatty acid ester containing from about 10 to 12 carbons in the acyl chain, and mixtures thereof.

4. The method of claim 1, wherein the slow release neutral lipid is selected from the group
10 consisting of triglycerides having a monounsaturated fatty acid ester containing from about 6 to 8 carbons in the acyl chain.

5. The method of claim 1, wherein the molar ratio of the slow release neutral lipid to the fast
15 release neutral lipid is in the range from about 1:1 to 1:100.

6. The method of claim 1, wherein the molar ratio of the slow release neutral lipid to the fast release neutral lipid is in the range from about 1:4 to
20 1:27.

7. The method of claim 1, wherein the slow
release neutral lipid is selected from the group consisting of triolein, tripalmitolein, trimyristolein, trilaurin, tricaprin, and mixtures thereof, and the fast
25 release neutral lipid is selected from the group consisting of tricaprylin, tricaproin, and mixtures thereof.

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8. The method of claim 1, wherein the slow release neutral lipid is tripalmitolein.

9. The method of claim 1, wherein the slow release neutral lipid is triolein.

5 10. The method of claim 1, wherein the slow release neutral lipid is tricaproin.

11. The method of claim 1, wherein the fast release neutral lipid is selected from the group
10 consisting of triglycerides having a saturated fatty acid ester containing from 6 to 8 carbons in the acyl chain.

12. The method of claim 1, wherein the fast release neutral lipid is selected from the group consisting of tricaprylin, tricaproin, and mixtures
15 thereof.

13. The method of claim 9, wherein the fast release neutral lipid is tricaprylin or a mixture of tricaprylin and tricaproin.

14. The method of claim 1, wherein the slow
20 release neutral lipid is selected from the group -
consisting of C8,C10 mixed acyl propylene glycol diesters and cholesterol esters and the fast release neutral lipid is tricaprylin or tricaproin.

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15. A method for modifying the rate of release of a biologically active compound encapsulated in a multivesicular liposome, said method comprising utilizing a blend of triolein or tripalmitolein and a fast release neutral lipid as the neutral lipid component in a multivesicular formulation in which an active compound is encapsulated;

wherein the rate of release of the biologically active compound increases in proportion with the molar ratio of the fast release neutral lipid to the triolein or tripalmitolein in the neutral lipid component.

16. The method of claim 15, wherein the rate of release is *in vivo*, and the neutral lipid component has a melting point about or below an *in vivo* temperature.

17. The method of claim 15, wherein the release is at storage temperature, and the melting point of the neutral lipid component is about or above the storage temperature.

18. The method of claim 15, wherein the fast release neutral lipid is selected from the group consisting of tricaprylin, tricaproin, and mixtures thereof.

19. The method of claim 15, wherein the fast release neutral lipid is tricaprylin, and the molar ratio of triolein or tripalmitolein to tricaprylin is in the range from about 1:1 to 1:100.

20. The method of claim 15, wherein the molar

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ratio of the triolein or tripalmitolein to the fast release neutral lipid is in the range from about 1:1 to 1:27.

21. The method of claim 15, wherein the release is *in vivo*, and the fast release neutral lipid is tricaprylin.

22. A method for selecting a multivesicular liposome formulation with a desired release rate of an encapsulated biologically active compound at a given temperature, said method comprising:

(a) preparing a family of multivesicular liposomal formulations wherein each member of the family is made by

(1) forming an emulsion from (i) a lipid component comprising an organic solvent, an amphipathic lipid, and a neutral lipid component comprising a molar ratio of from 1:0 to 0:1 of a slow release rate neutral lipid to a fast release rate neutral lipid, and (ii) an immiscible first aqueous component, wherein at least one biologically active compound is incorporated into either the lipid component or the first aqueous component, or both;

(2) mixing the emulsion with a second aqueous component to form solvent spherules, and

(3) removing the organic solvent from the solvent spherules to form multivesicular liposomes encapsulating the biologically active compound;

wherein for each member of the family the neutral lipid component has a different molar ratio of the slow release rate neutral lipid to the fast release rate neutral lipid;

(b) incubating each member of the family at a given temperature to obtain a family of release rate profiles; and

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(c) selecting the family member with the neutral lipid component yielding the desired release rate profile.

23. The method of claim 22, wherein the
5 amphipathic lipid is selected from the group consisting of 1,2-dioleoyl-*sn*-glycero-3-phosphocholine (DOPC), 1,2-distearoyl-*sn*-glycero-3-phosphocholine (DSPC), and 1,2-dierucoyl-*sn*-glycero-3-phosphocholine (DEPC), and the slow release neutral lipid is triolein or tripalmitolein.

10 24. The method of claim 22, wherein the fast release neutral lipid is tricaprylin.

25. The method of claim 22, wherein the molar ratio is selected in the range from about 1:1 to 1:54.

26. The method of claim 22, wherein the molar
15 ratio of the neutral lipid component to all the lipids in the lipid component is in the range from about 0.01 to about 0.21.

27. The method of claim 22, wherein the slow
release neutral lipid is selected from the group
20 consisting of triolein, tripalmitolein, trimyristolein, - trilaurin, tricaprin and mixtures thereof, and the fast release neutral lipid is selected from the group consisting of tricaprylin, tricaproin, and mixtures thereof.

25 28. The method of claim 27, wherein the molar ratio of the slow release neutral lipid to the fast release neutral lipid is in the range from about 1:1 to 1:54.

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29. The method of claim 22, wherein the release rate is *in vivo* and the slow release neutral lipid is triolein.

30. The method of claim 29, wherein the fast
5 release neutral lipid is tricaprylin.

31. The method of claim 22, wherein the amphipathic lipid is selected from the group consisting of

1,2-dioleoyl-*sn*-glycero-3-phosphocholine,
10 1,2-dilauroyl-*sn*-glycero-3-phosphocholine,
1,2-dimyristoyl-*sn*-glycero-3-phosphocholine,
1,2-dipalmitoyl-*sn*-glycero-3-phosphocholine,
1,2-distearoyl-*sn*-glycero-3-phosphocholine,
1,2-diarachidoyl-*sn*-glycero-3-phosphocholine,
15 1,2-dibehenoyl-*sn*-glycero-3-phosphocholine,
1,2-dipalmitoleoyl-*sn*-glycero-3-phosphocholine,
1,2-dieicosenoyl-*sn*-glycero-3-phosphocholine,
1,2-dierucoyl-*sn*-glycero-3-phosphocholine,
1,2-dipalmitoyl-*sn*-glycero-3-phosphoglycerol, and
20 1,2-dioleoyl-*sn*-glycero-3-phosphoglycerol.

32. A multivesicular liposome comprising:
a neutral lipid component having a molar
ratio of a slow release neutral lipid to a fast neutral
lipid in the range from about 1:1 to 1:100;
25 an amphipathic lipid; and
a biologically active compound encapsulated
in water in the liposome.

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33. The liposome of claim 32, wherein the melting point of the neutral lipid component is about or below 37°C.

34. The liposome of claim 32, wherein the slow
5 release neutral lipid is selected from the group consisting of triglycerides having a monounsaturated fatty acid ester with from about 14 to 18 carbons in the acyl chain, those having a saturated fatty acid ester with from about 10 to 12 carbons in the acyl chain, and
10 mixtures thereof.

35. The liposome of claim 32, wherein the slow release neutral lipid is selected from the group consisting of triolein, tripalmitolein, trimyristolein, trilaurin, tricaprln and mixtures thereof, and the fast
15 release neutral lipid is selected from the group consisting of tricaprylin, tricaproin, and mixtures thereof.

36. The liposome of claim 32, wherein the fast release neutral lipid is selected from the group
20 consisting of triglycerides having a saturated fatty acid ester with from about 6 to 8 carbons in the acyl chain. -

37. The liposome of claim 32, wherein the fast release neutral lipid is selected from the group consisting of tricaprylin and tricaproin, and mixtures
25 thereof.

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38. The liposome of claim 32, wherein the molar ratio of the neutral lipid component to all the lipids in the liposome is in the range from about 0.01 to about 0.21.

5 39. The liposome of claim 32, wherein the molar ratio of the slow release neutral lipid to the fast release neutral lipid is in the range from about 1:1 to 1:27.

 40. The liposome of claim 32, wherein the molar
10 ratio of the slow release neutral lipid to the fast release neutral lipid is in the range from about 1:1 to 1:18.

 41: A method for administering a biologically active compound at a desired release rate comprising
15 administering the liposome of claim 32 to a subject in need of the biologically active compound encapsulated therein.

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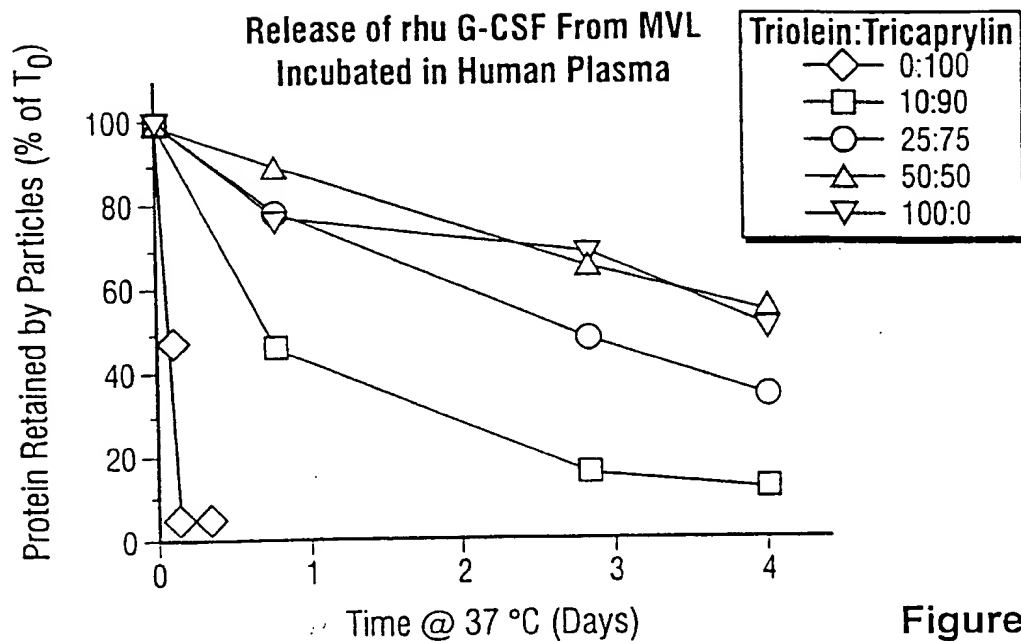


Figure 1

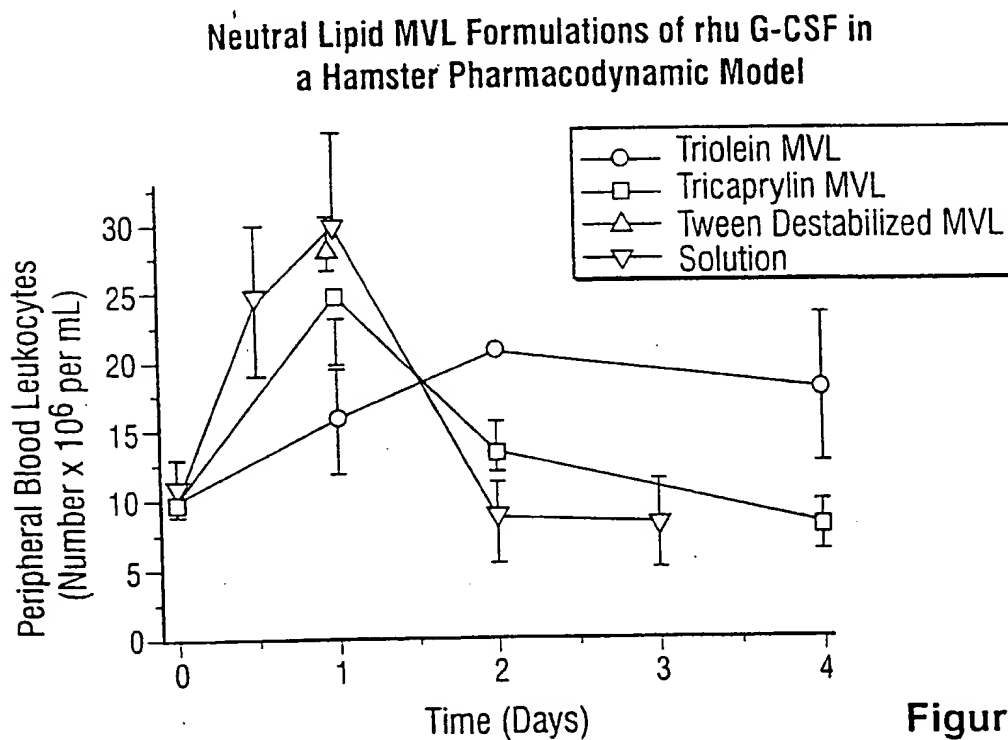


Figure 2

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Release of rhu GM-CSF from MVL
Incubated in Human Plasma

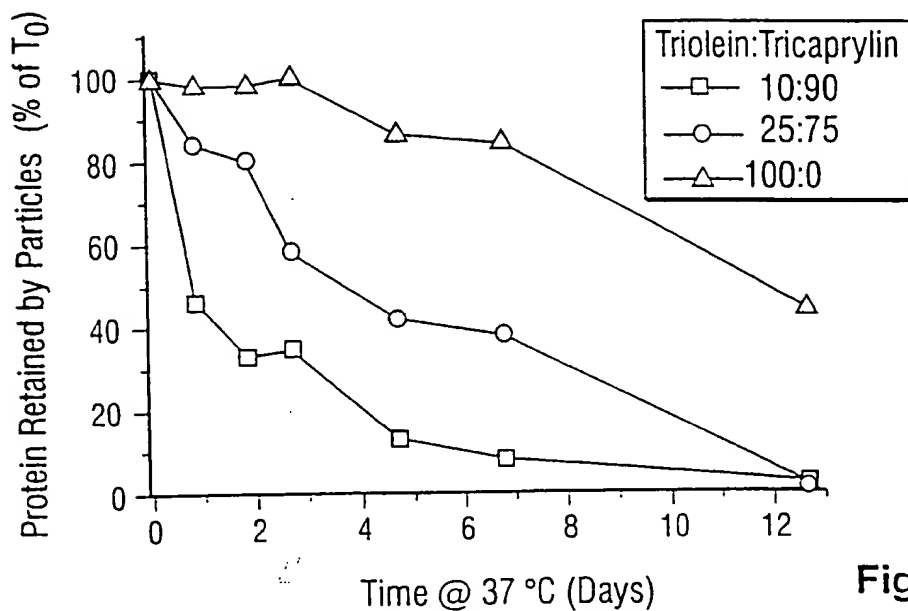


Figure 3

Neutral Lipid MVL Formulations of rhu GM-CSF in
a Marine Pharmacokinetic Model

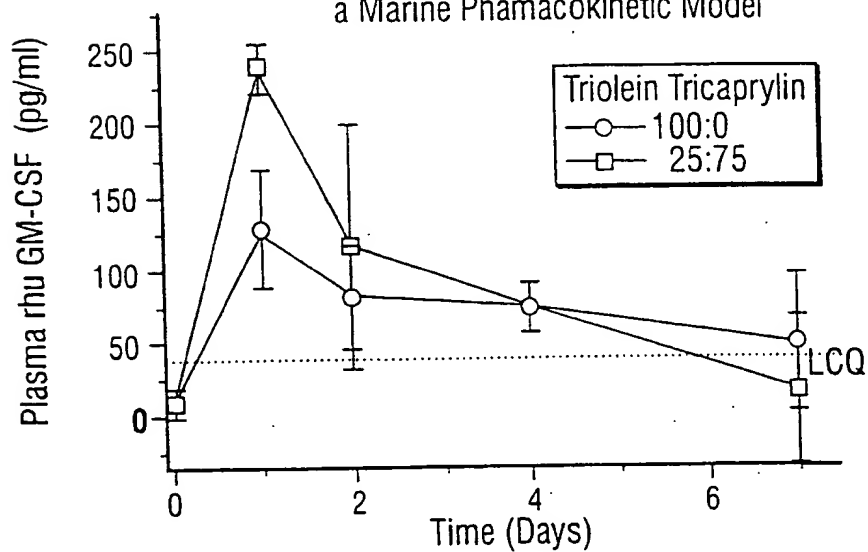


Figure 4

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Release of rhu IGF-1 in Human Plasma
From MVL Manufactured with Different Neutral Lipids

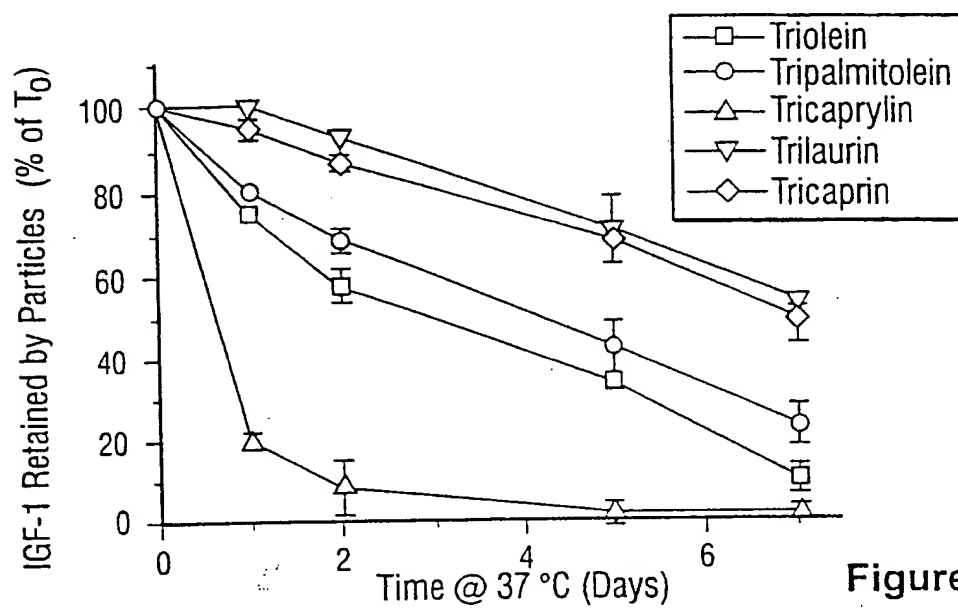


Figure 5

MVL Formulations of rhu IGF-1 in
a Rat Pharmacokinetic Model

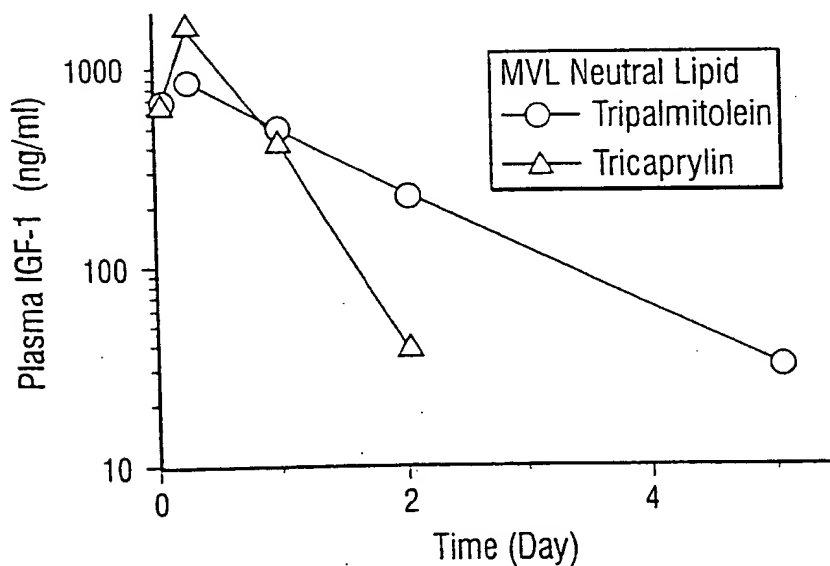


Figure 6

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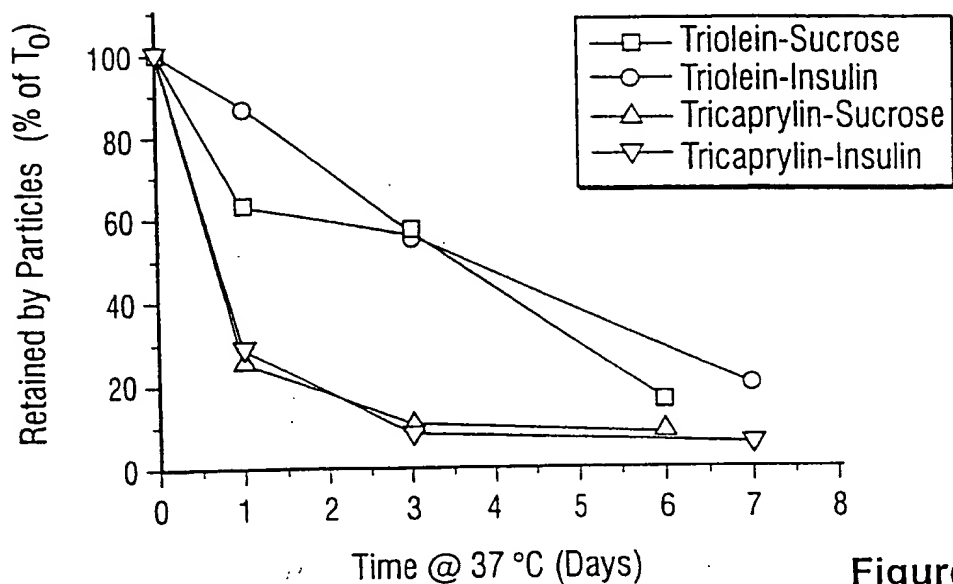
Release of rhu-Insulin (E coli) and ^{14}C -Sucrose
from MVL Incubated in Human Plasma

Figure 7

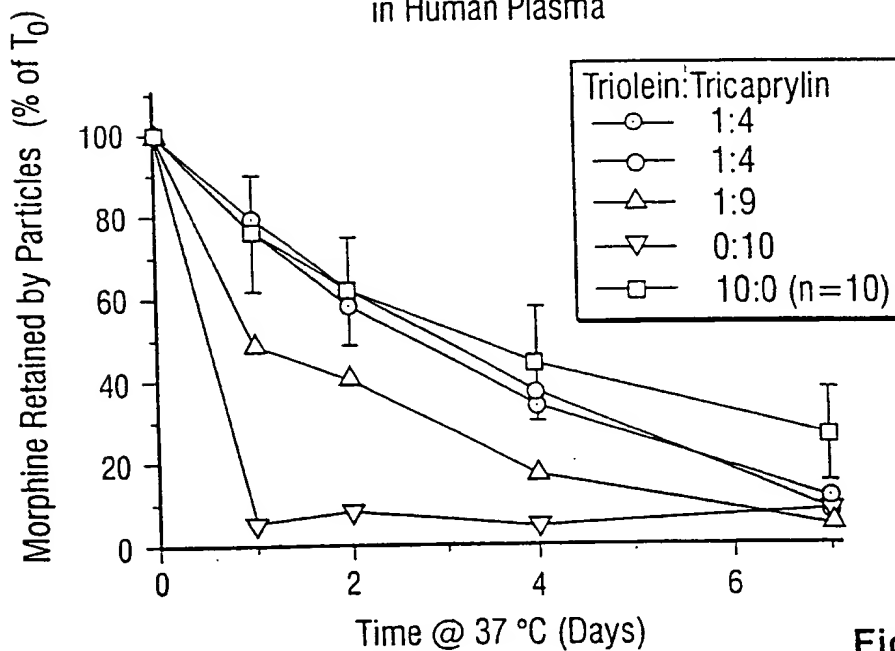
Release of Morphine From MVL Incubated
in Human Plasma

Figure 8

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Morphine Levels in Dog CSF Following Epidural Injection of
Morphine Sulfate in Different Neutral Lipid MVL Formulations

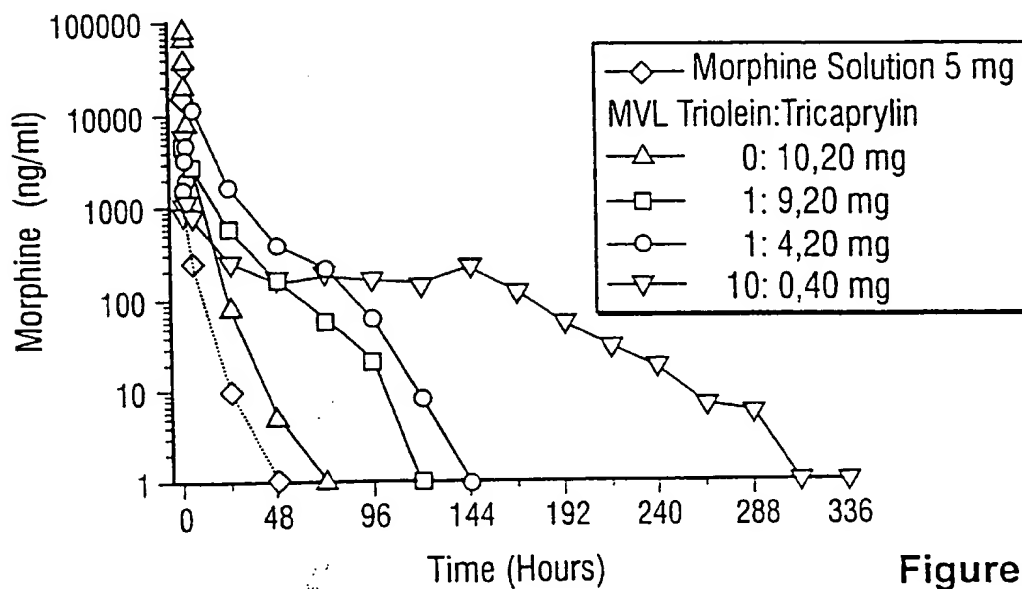


Figure 9

The Release Rate of Morphine MVL Formulations
Stored at Different Temperatures in Normal Saline Solutions

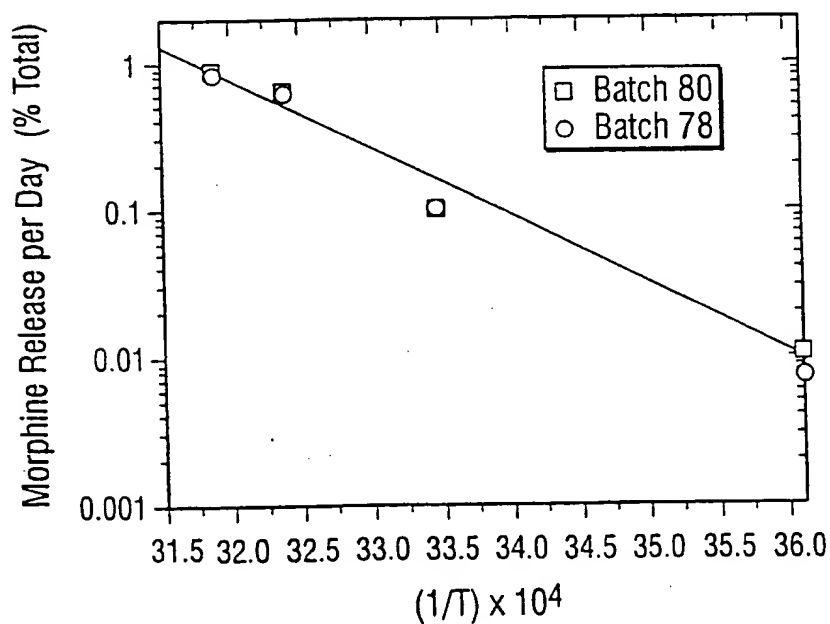


Figure 10

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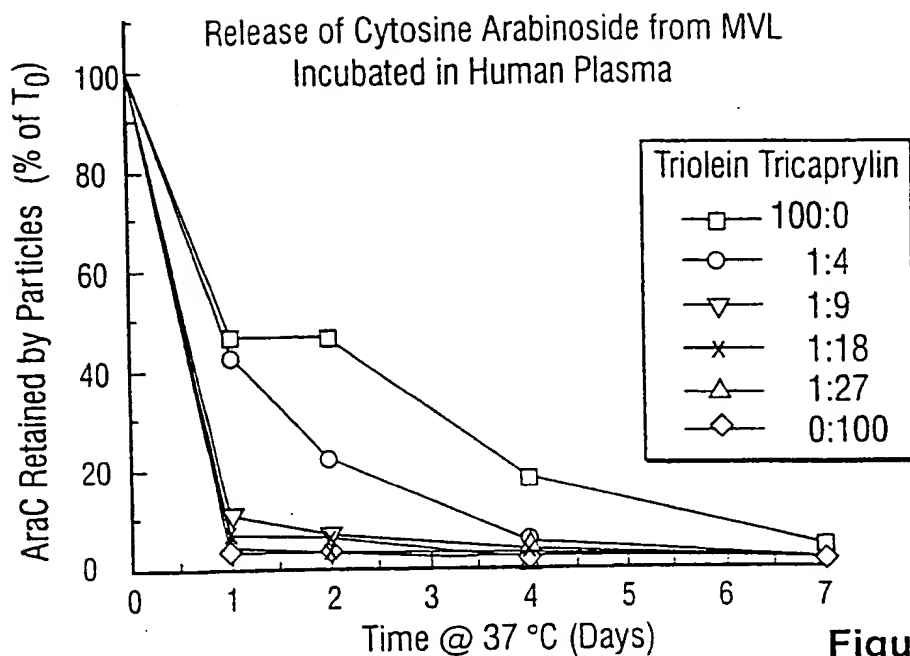


Figure 11

The Influence of Phospholipid Chain-Length Composition on the Neutral Lipids
Effect on MVL Release of Cytosine Arabinoside (AraC) in Human Plasma

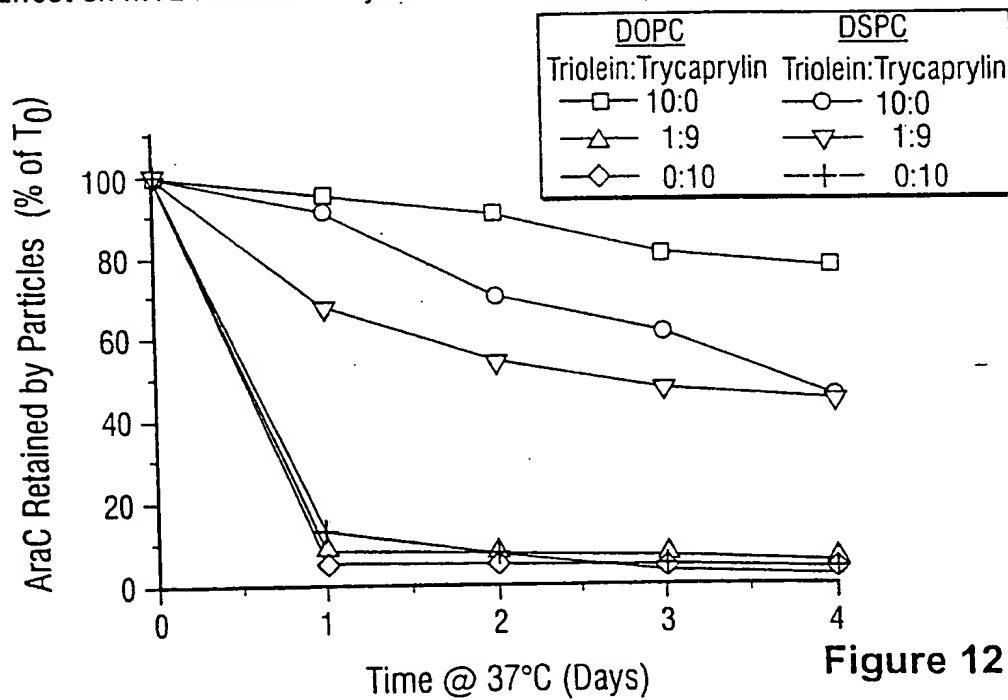
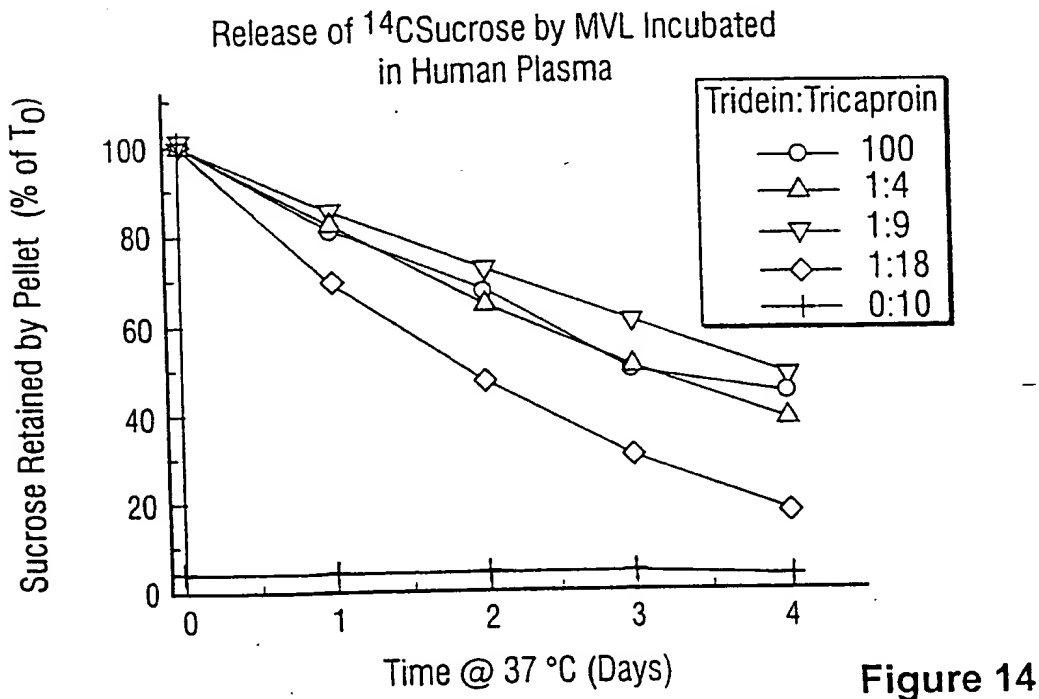
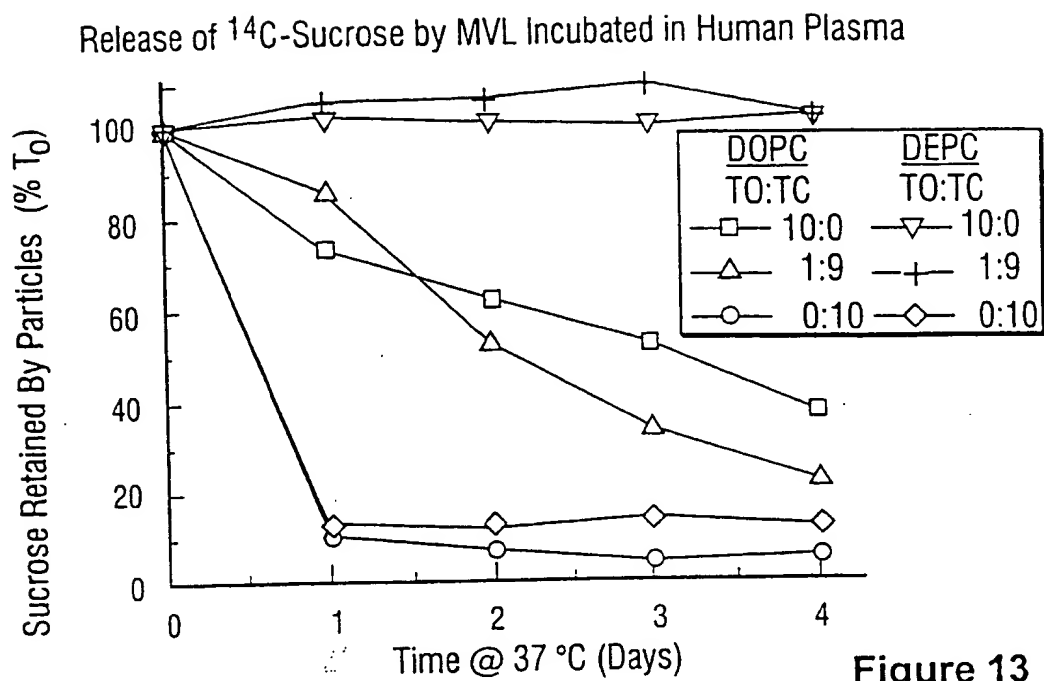


Figure 12

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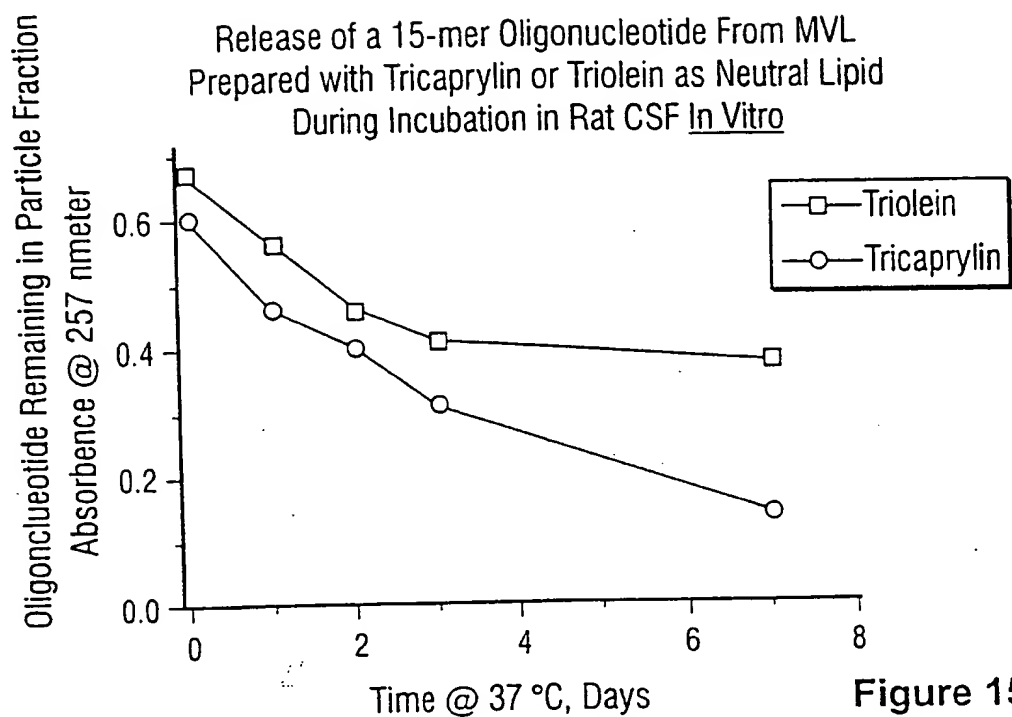


Figure 15

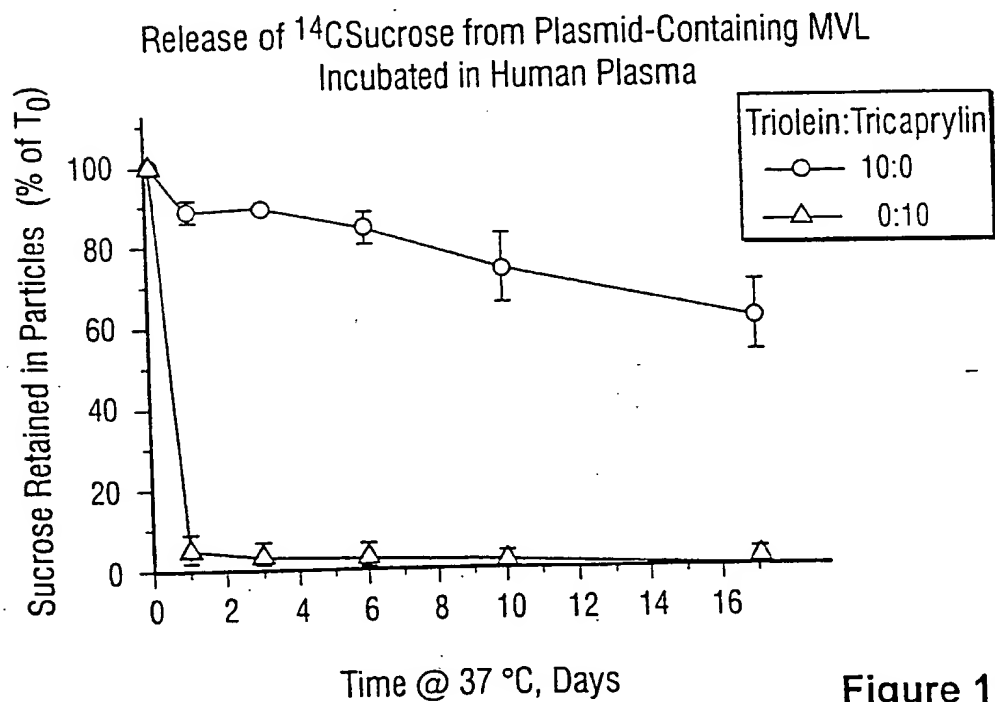


Figure 16

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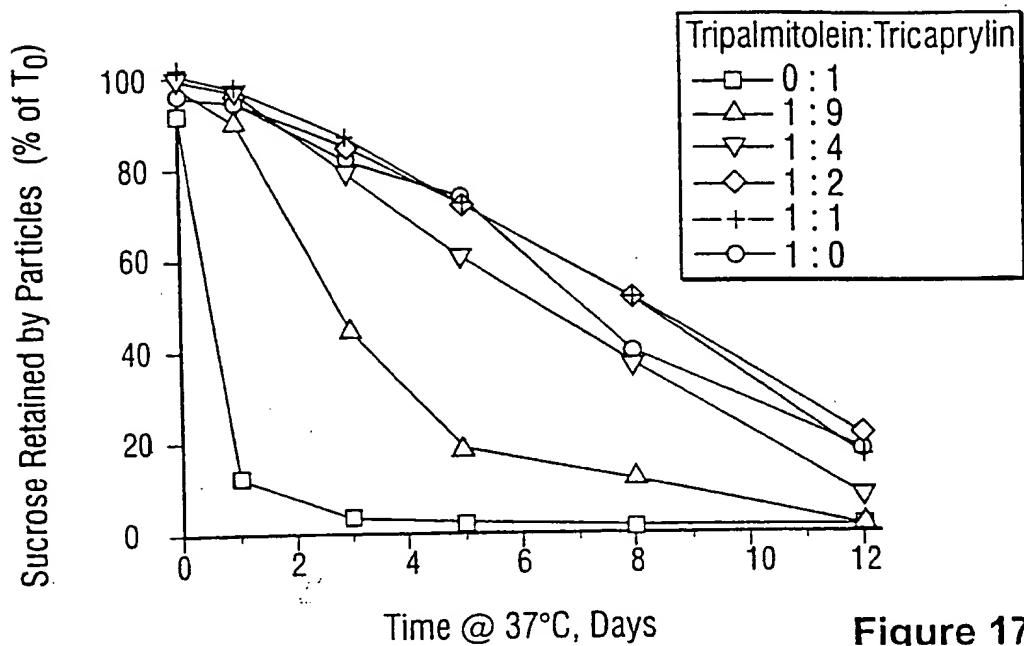
Release of ^{14}C -Sucrose From MVL Incubated
in Human Plasma

Figure 17

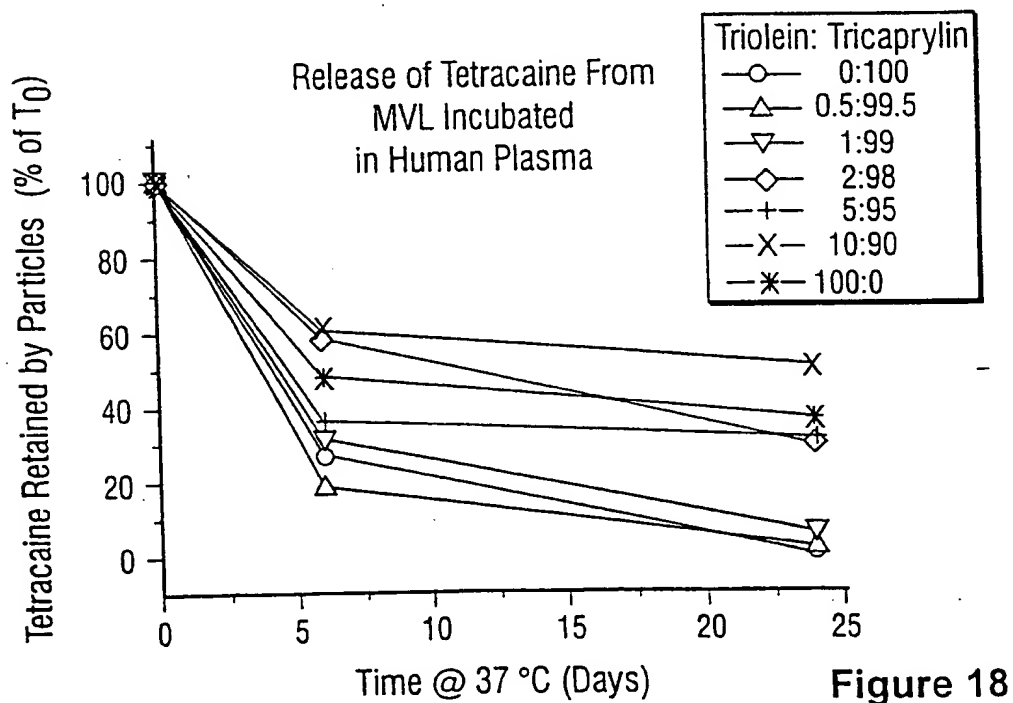


Figure 18

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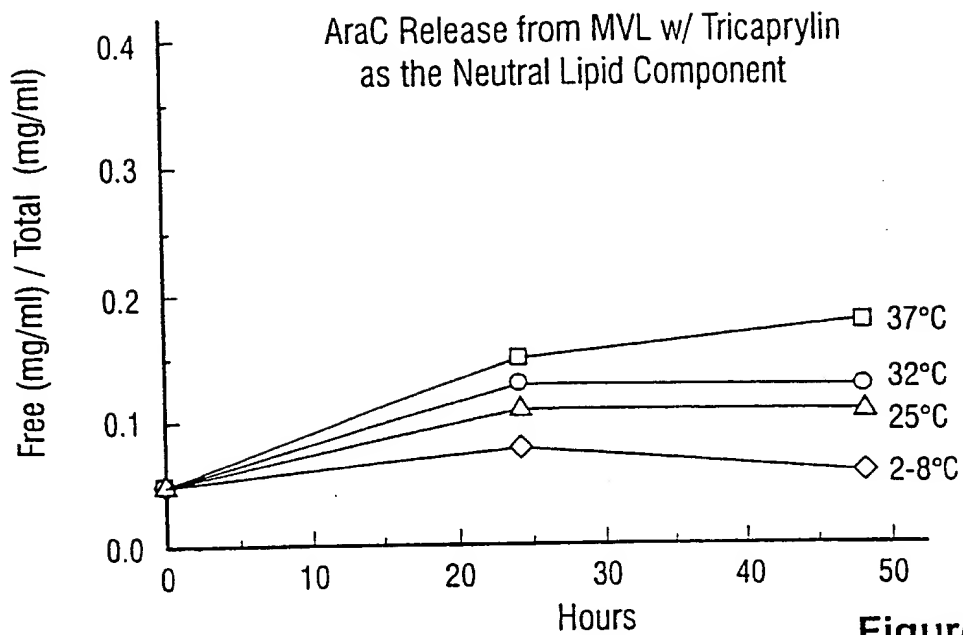


Figure 19A

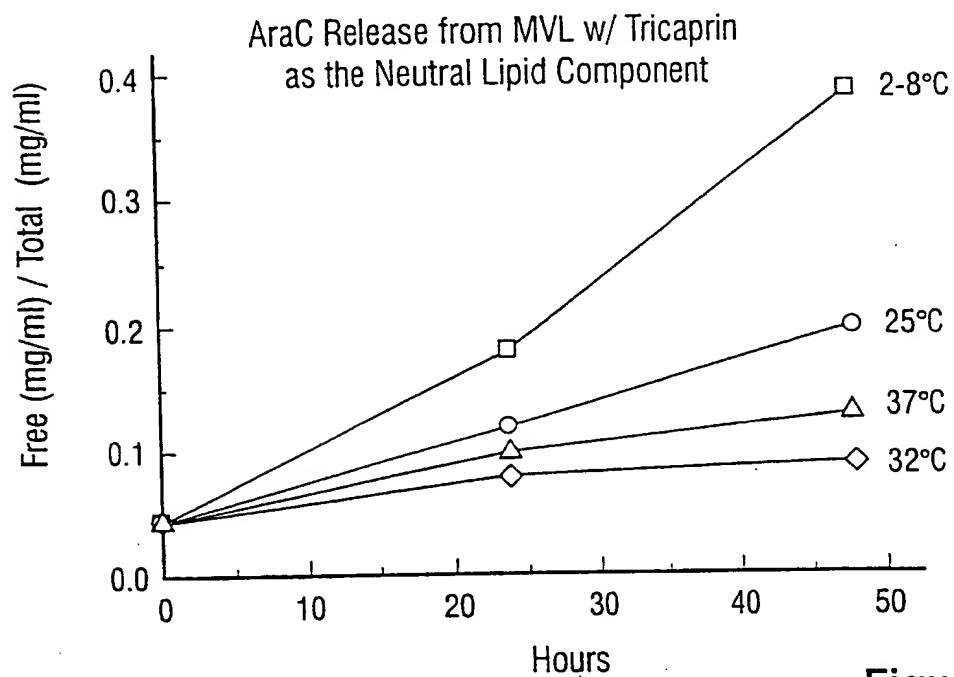


Figure 19B

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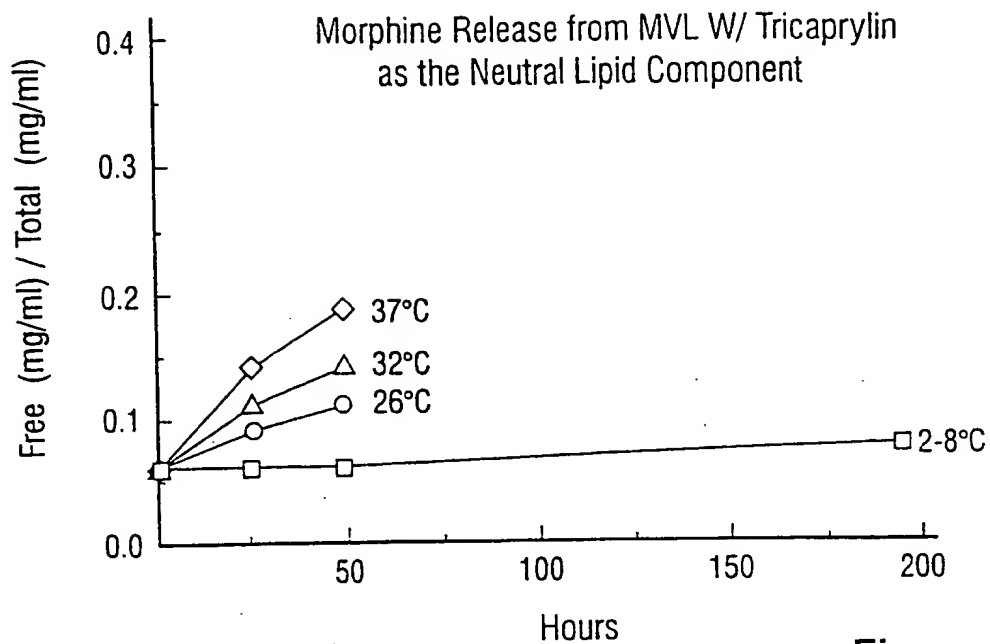


Figure 19C

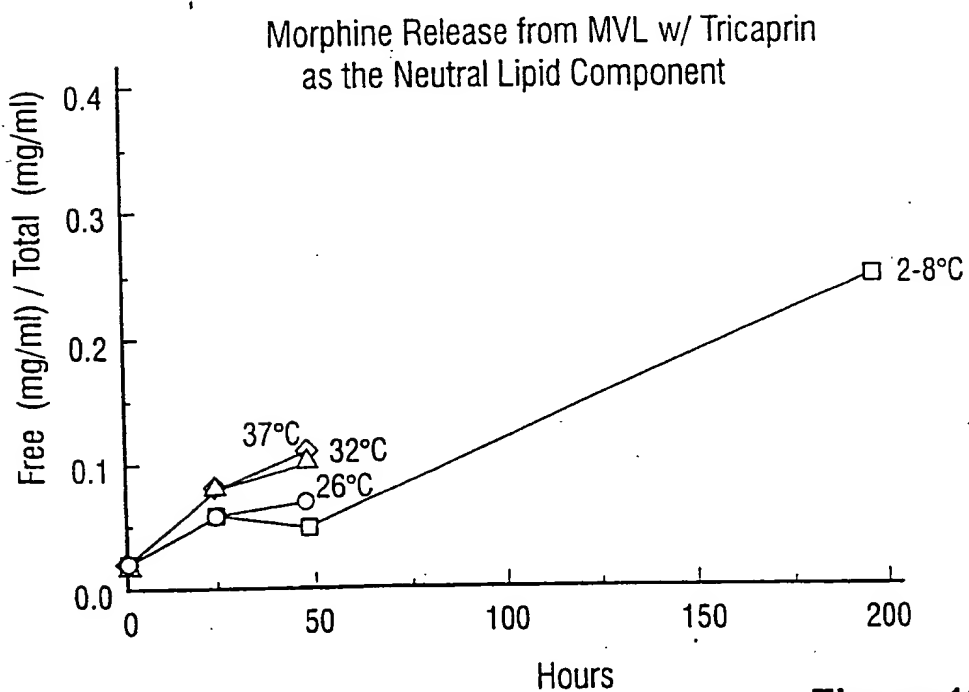


Figure 19D

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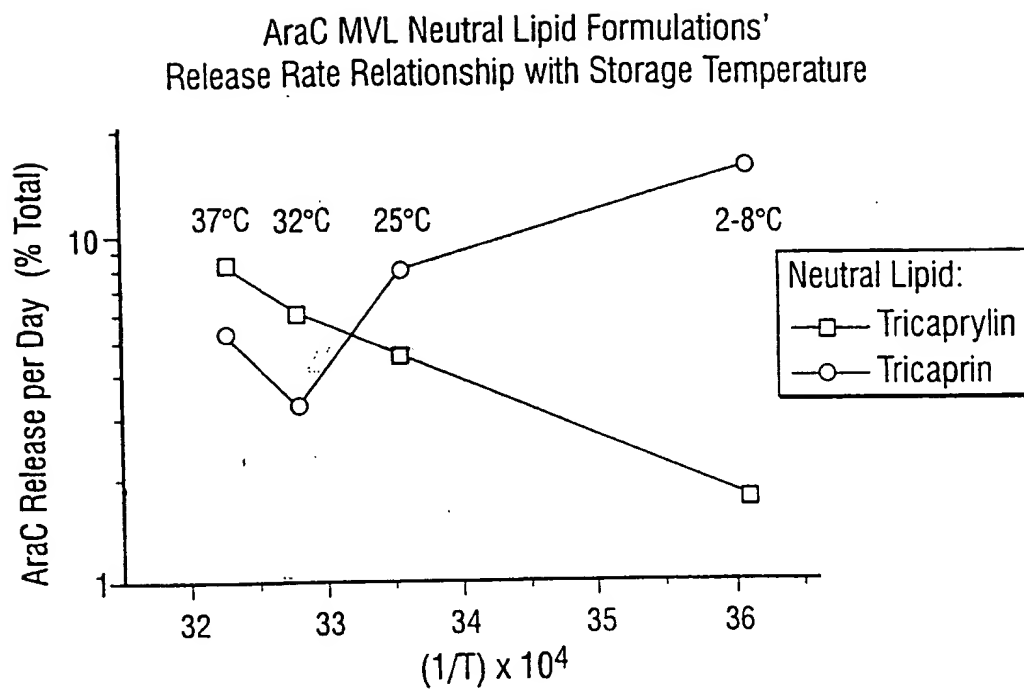


Figure 20

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US98/01636

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) : A61K 9/127, 9/133

US CL : 424/450

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 424/450; 264/4.1, 4.3

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched
NONE

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)
APS; Chemical Abstracts

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X — Y	US 5,422,120 A (KIM) 06 June 1995, Examples, especially 5 and 6.	1-7, 9-21, 32-35 & 38-41 ----- 8, 22-31 & 36-37

☐ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents:	* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
A document defining the general state of the art which is not considered to be of particular relevance	*X* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
B earlier document published on or after the international filing date	*Y* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
L document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	*G* document member of the same patent family
O document referring to an oral disclosure, use, exhibition or other means	
P document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

29 MARCH 1998

Date of mailing of the international search report

28 MAY 1998

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